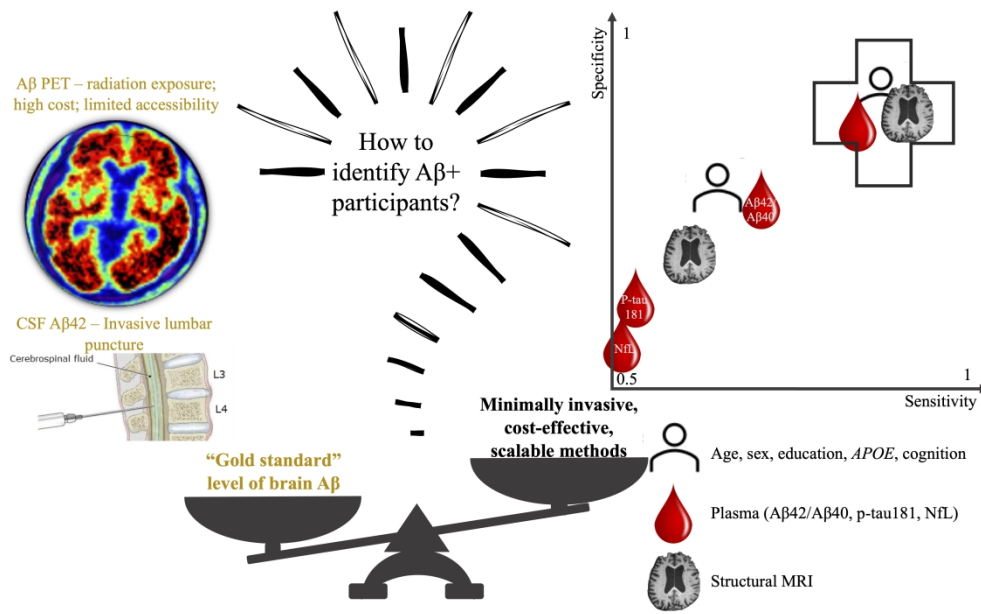


**Detection of  $\beta$ -amyloid positivity in ADNI with demographics, cognition, MRI, and plasma biomarkers**

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Keywords:	amyloid, plasma, PET, MRI, Alzheimer, P-tau181



Effective combinations of demographics, APOE genotype, global cognitive measures, MRI, and plasma biomarkers as promising minimally invasive and low-cost assessments to detect the Aβ-positivity using florbetapir PET status as the ground-truth.

336x207mm (300 x 300 DPI)

## STROBE statement: Reporting guidelines checklist for cohort, case-control and cross-sectional studies

SECTION	ITEM NUMBER	CHECKLIST ITEM	REPORTED ON PAGE NUMBER:
<b>TITLE AND ABSTRACT</b>			
	1a	Indicate the study's design with a commonly used term in the title or the abstract	1,3
	1b	Provide in the abstract an informative and balanced summary of what was done and what was found	3
<b>INTRODUCTION</b>			
Background and objectives	2	Explain the scientific background and rationale for the investigation being reported	5-7
	3	State specific objectives, including any pre-specified hypotheses	6-7
<b>METHODS</b>			
Study design	4	Present key elements of study design early in the paper	7
Setting	5	Describe the setting, locations, and relevant dates, including periods of recruitment, exposure, follow-up, and data collection	7-8
Participants	6a	Cohort study—Give the eligibility criteria, and the sources and methods of selection of participants. Describe methods of follow-up Case-control study—Give the eligibility criteria, and the sources and methods of case ascertainment and control selection. Give the rationale for the choice of cases and controls Cross-sectional study—Give the eligibility criteria, and the sources and methods of selection of participants	7-8
	6b	Cohort study—For matched studies, give matching criteria and number of exposed and unexposed Case-control study—For matched studies, give matching criteria and the number of controls per case Variables	N/A
Variables	7	Clearly define all outcomes, exposures, predictors, potential confounders, and effect modifiers. Give diagnostic criteria, if applicable	7-10
Data sources/measurements	8*	For each variable of interest, give sources of data and details of methods of assessment	7-10

SECTION	ITEM NUMBER	CHECKLIST ITEM	REPORTED ON PAGE NUMBER:
		(measurement). Describe comparability of assessment methods if there is more than one group.	
Bias	9	Describe any efforts to address potential sources of bias.	
Study size	10	Explain how the study size was arrived at	7-8
Quantitative variables	11	Explain how quantitative variables were handled in the analyses. If applicable, describe which groupings were chosen and why.	7-10
Statistical methods	12a	Describe all statistical methods, including those used to control for confounding	10-11
	12b	Describe any methods used to examine subgroups and interactions	10-11
	12c	Explain how missing data were addressed	N/A
	12d	Cohort study—If applicable, explain how loss to follow-up was addressed Case-control study—If applicable, explain how matching of cases and controls was addressed Cross-sectional study—If applicable, describe analytical methods taking account of sampling strategy	N/A
	12e	Describe any sensitivity analyses	10-11
<b>RESULTS</b>			
Participants	13a	Report numbers of individuals at each stage of study—eg numbers potentially eligible, examined for eligibility, confirmed eligible, included in the study, completing follow-up, and analysed	12
	13b	Give reasons for non-participation at each stage	N/A
	13c	Consider use of a flow diagram	N/A
Descriptive Data	14a	Give characteristics of study participants (eg demographic, clinical, social) and information on exposures and potential confounders	12
	14b	Indicate number of participants with missing data for each variable of interest	N/A
	14c	Cohort study—Summarise follow-up time (eg, average and total amount)	N/A
Outcome Data	15*	Cohort study—Report numbers of outcome events or summary measures over time Case-control study—Report numbers in each exposure category, or summary measures of exposure Cross-sectional study—Report numbers of outcome events or summary measures	12

SECTION	ITEM NUMBER	CHECKLIST ITEM	REPORTED ON PAGE NUMBER:
Main Results	16a	Give unadjusted estimates and, if applicable, confounder-adjusted estimates and their precision (e.g. 95% confidence interval). Make clear which confounders were adjusted for and why they were included	13-15
	16b	Report category boundaries when continuous variables were categorized	13-15
	16c	If relevant, consider translating estimates of relative risk into absolute risk for a meaningful time period	N/A
	16d	Report results of any adjustments for multiple comparisons	N/A
Other Analyses	17a	Report other analyses done—e.g. analyses of subgroups and interactions, and sensitivity analyses	Supp Material
	17b	If numerous genetic exposures (genetic variants) were examined, summarize results from all analyses undertaken	N/A
	17c	If detailed results are available elsewhere, state how they can be accessed	13-15
<b>DISCUSSION</b>			
Key Results	18	Summarise key results with reference to study objectives	15
Limitations	19	Discuss limitations of the study, taking into account sources of potential bias or imprecision. Discuss both direction and magnitude of any potential bias	22
Interpretation	20	Give a cautious overall interpretation of results considering objectives, limitations, multiplicity of analyses, results from similar studies, and other relevant evidence	22-23
Generalisability	21	Discuss the generalisability (external validity) of the study results Other information	22-23
<b>FUNDING</b>			
	22	Give the source of funding and the role of the funders for the present study and, if applicable, for the original study on which the present article is based	24

\*Give information separately for cases and controls in case-control studies and, if applicable, for exposed and unexposed groups in cohort and cross-sectional studies.

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4 **Abbreviated Summary:** Tosun et al. report a systematic comparison of A $\beta$ -positivity detection  
5 models, identifying effective combinations of demographics, *APOE* genotype, global cognitive  
6 measures, MRI, and plasma biomarkers as promising minimally invasive and low-cost  
7 assessments to detect the A $\beta$ -positivity using florbetapir PET status as the ground-truth.  
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4 **Detection of  $\beta$ -amyloid positivity in ADNI with demographics, cognition, MRI,**  
5 **and plasma biomarkers**  
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10 Duygu Tosun<sup>1,2</sup>, Dallas Veitch<sup>2</sup>, Paul Aisen<sup>3</sup>, Clifford R. Jack, Jr.<sup>4</sup>, William J. Jagust<sup>5</sup>,  
11 Ronald C. Petersen<sup>6,7</sup>, Andrew J Saykin<sup>8,9,10</sup>, James Bollinger<sup>11,12</sup>, Vitaliy Ovod<sup>11,12</sup>,  
12 Kwasi G. Mawuenyega<sup>11,12</sup>, Randall J. Bateman<sup>11,12, 13</sup>, Leslie M. Shaw<sup>14</sup>, John Q.  
13 Trojanowski<sup>14</sup>, Kaj Blennow<sup>15,16</sup>, Henrik Zetterberg<sup>15,16,17,18</sup>, and Michael W. Weiner<sup>1,2</sup>, for the  
14 Alzheimer's Disease Neuroimaging Initiative\*  
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13 \*Data used in preparation of this article were obtained from the Alzheimer's Disease  
14 Neuroimaging Initiative (ADNI) database (adni.loni.usc.edu). As such, the investigators within  
15 the ADNI contributed to the design and implementation of ADNI and/or provided data but did  
16 not participate in analysis or writing of this report. A complete listing of ADNI investigators can  
17 be found at: [http://adni.loni.usc.edu/wp-](http://adni.loni.usc.edu/wp-content/uploads/how_to_apply/ADNI_Acknowledgement_List.pdf)  
18 [content/uploads/how\\_to\\_apply/ADNI\\_Acknowledgement\\_List.pdf](http://adni.loni.usc.edu/wp-content/uploads/how_to_apply/ADNI_Acknowledgement_List.pdf)  
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## Abbreviations

A $\beta$	$\beta$ -amyloid
AD	Alzheimer's disease
ADAS-Cog	Alzheimer's Disease Assessment Scale – Cognitive subscale
ADNI	Alzheimer's Disease Neuroimaging Initiative
AUC	area under curve
CDR-SB	Clinical Dementia Rating – Sum of Boxes
CI	cognitively impaired
CSF	cerebrospinal fluid
CU	cognitively unimpaired
DL	deep learning
FDG	fluorodeoxyglucose
LC-MS/MS	liquid chromatography tandem mass spectrometry
LONI	Laboratory of Neuro Imaging
MMSE	Mini-Mental State Examination
MRI	magnetic resonance imaging
MSD	Meso Scale Discovery
NfL	neurofilament light
NPV	negative predictive value
PET	positron emission tomographic
PPV	positive predictive value
RF	random forest
Simoa	Single molecule array
SUVr	standardized uptake value ratio

## Abstract

*In vivo* gold standard for the ante-mortem assessment of brain  $\beta$ -amyloid( $A\beta$ ) pathology is currently  $A\beta$  positron emission tomography(PET) or cerebrospinal fluid(CSF) measures of  $A\beta_{42}$  or the  $A\beta_{42}/A\beta_{40}$  ratio. The widespread acceptance of a biomarker classification scheme for the Alzheimer's disease(AD) continuum has ignited interest in more affordable and accessible approaches to detect AD  $A\beta$  pathology, a process that often slows down the recruitment into, and adds to the cost of, clinical trials. Many evaluated the role of demographics, cognition, and magnetic resonance imaging(MRI) to predict AD  $A\beta$  pathology. More recently there has been considerable excitement concerning the value of blood biomarkers. Leveraging multidisciplinary data from cognitively unimpaired(CU) participants and participants with mild cognitive impairment(CI) recruited by the multisite biomarker study of Alzheimer's Disease Neuroimaging Initiative(ADNI), here we assessed to what extent plasma  $A\beta_{42}/A\beta_{40}$ , neurofilament light(NfL), and p-tau181 biomarkers detect presence of AD  $A\beta$  pathology, and to what extent the addition of clinical information such as demographic data, *APOE* genotype, cognitive assessments, and MRI can assist plasma biomarkers in detecting  $A\beta$ -positivity. Our results confirm plasma  $A\beta_{42}/A\beta_{40}$  as a robust biomarker of brain  $A\beta$ -positivity(AUC of 0.80–0.87). Plasma p-tau181 detected  $A\beta$ -positivity only in the CIs with a moderate AUC of 0.67, while plasma NfL did not detect  $A\beta$ -positivity in either group of participants. Clinical information as well as MRI-score independently detected PET  $A\beta$ -positivity both in CU and CIs(AUC of 0.69–0.81). Clinical information, particularly *APOE*  $\epsilon 4$  status, enhanced performance of plasma biomarkers in the detection of PET  $A\beta$ -positivity by 0.06–0.14 units of AUC for CUs, and by 0.21–0.25 units for CIs; and further enhancement of these models with an MRI-score of  $A\beta$ -positivity yielded an additional improvement of 0.04–0.11 units of AUC for CU participants and 0.05–0.09 units for CIs. Taken together, these multidisciplinary results suggest that when combined with clinical information, plasma P-tau181 and NfL biomarkers, and an MRI-score could effectively identify  $A\beta+$  CUs and CIs(AUC of 0.80–0.90). Yet, when the MRI-score is considered in combination with clinical information, plasma P-tau181 and plasma NfL have minimal added value for detecting brain  $A\beta$ -positivity in this multicenter ADNI cohort of CUs and CIs. Our systematic comparison of  $A\beta$ -positivity detection models identified effective combinations of demographics, *APOE* genotype, global cognitive measures, MRI, and plasma biomarkers.

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3 Promising minimally invasive and low-cost predictors such as plasma biomarkers of  $A\beta_{42}/A\beta_{40}$   
4 may be improved by age and *APOE* genotype.  
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## Introduction

Alzheimer's disease (AD), pathologically defined as the presence of plaques of  $\beta$ -amyloid ( $A\beta$ ) protein, neurofibrillary tangles of tau protein, and neurodegeneration (DeTure and Dickson, 2019), is the major cause of cognitive decline and dementia (2020). Currently, no treatment is approved that has been demonstrated to slow the progress of AD (Aisen, 2019). Historically, AD was diagnosed clinically through neurological and neuropsychological examinations to assess memory impairment and other thinking skills, judge functional abilities, and identify behavior changes, and exclude other causes than AD that could account for the dementia (McKhann *et al.*, 2011). The "gold-standard" method to confirm the presence of AD pathology is pathological examination of brains at autopsy (DeTure and Dickson, 2019). Since the turn of the century, the ability to diagnose AD pathology in living people has been made possible by the development of radioligands for  $A\beta$  positron emission tomographic (PET) scans (Klunk *et al.*, 2004; Schilling *et al.*, 2016) and tau PET scans (Marquie *et al.*, 2015; Leuzy *et al.*, 2019), magnetic resonance imaging (MRI) for neurodegeneration (Frisoni *et al.*, 2010), and analysis of cerebrospinal fluid (CSF) for  $A\beta$  and tau species (Blennow, 2004; Holtzman, 2011). This has led to an *in vivo* biological framework of AD including  $A\beta$ , tau and neurodegeneration, based on the so called A/T/N system (Jack *et al.*, 2018). Indeed, the descriptive A/T/N system places  $A\beta$ + individuals firmly on the AD continuum while individuals with  $A\beta$ - profiles are considered either normal or possessing non-AD pathologic changes (Jack *et al.*, 2018). Many trials, particularly the ones enrolling subjects in earlier stages of disease, are therefore using either  $A\beta$  PET imaging or CSF  $A\beta_{42}$  levels as a critical step in clinical trial cohort enrichment (Sperling *et al.*, 2014; Honig *et al.*, 2018).

Despite these advances, PET scans are quite costly and not universally accessible. Even though lumbar punctures are very safe (Peskind *et al.*, 2009), there continues to be reluctance to CSF sample collection in the patient and professional population (Moulder *et al.*, 2017). Therefore, there has been great interest in developing low cost, minimally invasive methods to detect AD  $A\beta$  pathology compared to PET scans and or CSF as the "gold standard". Many publications, (reviewed in Veitch *et al.*) have evaluated the role of demographics (Insel *et al.*, 2016; Tosun *et al.*, 2016; Jansen *et al.*, 2018; Buckley *et al.*, 2019; Ko *et al.*, 2019; Maserejian *et al.*, 2019),

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3 *APOE*  $\epsilon$ 4 (de Rojas *et al.*, 2018; Jansen *et al.*, 2018; Ten Kate *et al.*, 2018; Ba *et al.*, 2019;  
4 Buckley *et al.*, 2019), cognition (Mielke *et al.*, 2012; Burnham *et al.*, 2014; Kandel *et al.*, 2015;  
5 Burnham *et al.*, 2016; Insel *et al.*, 2016; Kim *et al.*, 2018; Lee *et al.*, 2018; Ba *et al.*, 2019;  
6 Brunet *et al.*, 2019; Maserejian *et al.*, 2019; Ansart *et al.*, 2020), and MRI measures (Tosun *et al.*  
7 *et al.*, 2013; Tosun *et al.*, 2014; Tosun *et al.*, 2016; Ten Kate *et al.*, 2018; Petrone *et al.*, 2019;  
8 Ansart *et al.*, 2020; Ezzati *et al.*, 2020) to detect AD A $\beta$  pathology. More recently there has been  
9 considerable excitement concerning the value of assays of plasma A $\beta$  species and related  
10 proteins (Burnham *et al.*, 2014; Kaneko *et al.*, 2014; Burnham *et al.*, 2016; Fandos *et al.*, 2017;  
11 Ovod *et al.*, 2017a; Park *et al.*, 2017; de Rojas *et al.*, 2018; Nakamura *et al.*, 2018; Verberk *et al.*  
12 *et al.*, 2018; Westwood *et al.*, 2018; Chatterjee *et al.*, 2019; Chen *et al.*, 2019; Goudey *et al.*, 2019;  
13 Lin *et al.*, 2019; Palmqvist *et al.*, 2019a; Palmqvist *et al.*, 2019b; Park *et al.*, 2019; Perez-  
14 Grijalba *et al.*, 2019; Vergallo *et al.*, 2019), species of plasma tau, including phosphorylated tau  
15 (p-tau) forms (Mielke *et al.*, 2018; Palmqvist *et al.*, 2019b; Barthélemy *et al.*, 2020; Janelidze *et al.*  
16 *et al.*, 2020a; Karikari *et al.*, 2020; Palmqvist *et al.*, 2020; Thijssen *et al.*, 2020), and plasma  
17 neurofilament light (NfL) (Palmqvist *et al.*, 2019b; Thijssen *et al.*, 2020) to detect AD A $\beta$   
18 pathology. The first reports of reproducible high precision, high accuracy tests of plasma  
19 A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> indicated high sensitivity and specificity for A $\beta$  plaques as measured by mass  
20 spectrometry (Ovod *et al.*, 2017b; Nakamura *et al.*, 2018). Subsequently, plasma measures of p-  
21 tau at residues 181 (Mielke *et al.*, 2018) and 217 (Barthélemy *et al.*, 2020; Palmqvist *et al.*,  
22 2020) indicated good performance relative to A $\beta$  plaques and tau tangles. The performance of  
23 these tests are being evaluated and have been shown to detect PET A $\beta$ -positivity conversion  
24 (Schindler *et al.*, 2019), be associated with cognitive decline, and correlate with AD pathology  
25 (Janelidze *et al.*, 2020a). If proven useful, these alternative approaches to detect AD A $\beta$   
26 pathology may play an important role in drug discovery and in accelerating identification of risk  
27 factors for AD with greater precision.

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48 For optimal and generalizable operationalization of such imputation approaches for the presence  
49 of AD A $\beta$  pathology, it is important to assess the independent and added value of each class of  
50 predictors (e.g., demographics, *APOE*  $\epsilon$ 4, cognition, plasma biomarkers, MRI, etc.) and the  
51 differences in their classification performances at different clinical stages. The Alzheimer's  
52 Disease Neuroimaging Initiative (ADNI) is a large, multisite, longitudinal study aimed at  
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3 validating biomarkers for AD clinical trials (Weiner *et al.*, 2017). ADNI participants have A $\beta$   
4 PET scans, lumbar punctures for CSF, and blood drawn for plasma studies, therefore allowing  
5 for a head-to-head comparison. This study specifically aimed to assess 1) to what extent plasma  
6 A $\beta_{42}$ /A $\beta_{40}$ , NfL, and P-tau181 biomarkers detect presence of AD A $\beta$  pathology (i.e., A $\beta$ -  
7 positivity); 2) to what extent the addition of demographic data, *APOE* genotype, and cognitive  
8 assessments and 3) MRI can assist plasma biomarkers in detecting A $\beta$ -positivity; and 4) to what  
9 extent the stage of clinical diagnosis affects these relationships.  
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## 17 **Materials and methods**

### 18 **Study design**

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21 Data used in the preparation of this article were obtained from the ADNI database  
22 (adni.loni.usc.edu). The ADNI was launched in 2003 as a public-private partnership, led by  
23 Principal Investigator Michael W. Weiner, MD. The primary goal of ADNI has been to test  
24 whether serial MRI, PET, other biological markers, and clinical and neuropsychological  
25 assessment can be combined to measure the progression of mild cognitive impairment (MCI) and  
26 early AD. For up-to-date information, see [www.adni-info.org](http://www.adni-info.org).  
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### 34 **Cohort**

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37 Subjects of this study were ADNI participants with known PET A $\beta$  status and with plasma  
38 biomarker assessments for p-tau181, and NfL, clinical assessments, and structural MRI within  
39 six months of A $\beta$  PET imaging. A subset of the main study cohort also had plasma biomarker  
40 assessment for A $\beta_{42}$ /A $\beta_{40}$ . The primary focus of the current study was to assess imputation of A $\beta$   
41 positivity from single time-point observations of clinical, neuroimaging, and plasma biomarker  
42 data; therefore, a cross-sectional study design was used. Although longitudinal biomarkers,  
43 neuroimaging, and clinical data are available for many ADNI participants, we considered only  
44 data from the first time-point with complete clinical, neuroimaging, and biomarker assessments  
45 for each participant to avoid circular model training and assessment. Clinical assessment closest  
46 in time to A $\beta$  PET imaging was used to define cognitively unimpaired (CU) and impaired (CI)  
47 diagnostic groups. The diagnostic criteria for ADNI participants were previously described  
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(Petersen *et al.*, 2010). Participant selection was made *a priori* from all ADNI subjects based on the availability of complete cross-sectional data as of June 30<sup>th</sup>, 2020.

### **PET A $\beta$ status**

Mean tracer uptake in the cerebellar gray and white matter was computed and used as reference to generate whole-brain standardized uptake value ratio (SUVR) maps of florbetapir PET scans (Jagust *et al.*, 2015). A composite region-of-interest consisting of middle frontal, anterior cingulate, posterior cingulate, inferior parietal, precuneus, supramarginal, middle temporal, and superior temporal regions was used to compute a global SUVR for florbetapir. A threshold of SUVR  $\geq$  1.11 for florbetapir (Landau *et al.*, 2013) was then used to determine PET A $\beta$  status.

### **Demographics data**

Age at florbetapir PET imaging, sex, and years of education were included as demographic characteristics of each participant.

### **Apolipoprotein E (APOE) genotyping**

*APOE* genotyping was done by the ADNI Genetics Core using DNA from blood samples, as detailed in Supplementary Material. *APOE*  $\epsilon$ 4 carrier status was considered as a predictor of A $\beta$ -positivity in this study.

### **Global cognitive assessments**

ADNI participants were assessed with a wide spectrum of clinical and cognitive tests (Weiner *et al.*, 2017). In this study, we limited the global cognitive assessments to the Clinical Dementia Rating – Sum of Boxes (CDR–SB), the Alzheimer's Disease Assessment Scale – Cognitive subscale 13-item (ADAS–Cog), and the Mini–Mental State Examination (MMSE) based on a 30-point questionnaire.

### **Plasma sample collection**

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3 Blood samples were obtained by venipuncture in EDTA tubes for plasma, following the ADNI  
4 protocol (Kang *et al.*, 2015). Within 60min, the samples were centrifuged at 3,000 r.p.m. at room  
5 temperature, aliquoted and stored at  $-80^{\circ}\text{C}$ . Samples underwent two freeze/thaws. Further  
6 details are provided in Supplementary Material.  
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### 10 11 **Plasma $\text{A}\beta_{42}$ and $\text{A}\beta_{40}$**

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14 Plasma  $\text{A}\beta$  isoform concentrations were determined using immunoprecipitation combined with  
15 liquid chromatography tandem mass spectrometry (LC-MS/MS) as previously described (Ovod  
16 *et al.*, 2017b). Plasma aliquots were thawed at  $21^{\circ}\text{C}/800$  RPM for 10 minutes and centrifuged at  
17  $21^{\circ}\text{C}/10000$  RCF for 5 minutes prior to immunoprecipitation. Targeted  $\text{A}\beta_{42}$  and  $\text{A}\beta_{40}$  isoforms  
18 were immunoprecipitated with an anti- $\text{A}\beta$  mid-domain antibody (HJ5.1) using a KingFisher  
19 (Thermo) automated immunoprecipitation platform. Immuno-enriched fractions were  
20 subsequently digested with Lys-N protease, generating  $\text{A}\beta_{28-42}$  and  $\text{A}\beta_{28-40}$  species, which were  
21 measured by LC-MS/MS (Ovod *et al.*, 2017b). Absolute  $\text{A}\beta$  isoform concentrations were  
22 determined with a  $^{15}\text{N}$ -labeled internal standard for each isoform. The total levels of  $\text{A}\beta_{42}$  and  
23  $\text{A}\beta_{40}$  were used to calculate the  $\text{A}\beta_{42}/\text{A}\beta_{40}$  ratio.  
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### 33 **Plasma p-tau181**

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35 Plasma p-tau181 was analyzed by the Single molecule array (Simoa) technique (Quanterix,  
36 Billerica, MA), using an assay developed in the Clinical Neurochemistry Laboratory, University  
37 of Gothenburg, Sweden (Karikari *et al.*, 2020). The assay uses a combination of two monoclonal  
38 antibodies (Tau12 and AT270) and measures N-terminal to mid-domain forms of pTau181  
39 (Karikari *et al.*, 2020). Calibrators were run as duplicates, while plasma samples were measured  
40 in singlicate. All the available samples were analyzed in a single batch.  
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### 47 **Plasma NfL**

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49 Plasma NfL was analyzed by the Simoa technique (Quanterix, Billerica, MA). The assay uses a  
50 combination of monoclonal antibodies, and purified bovine NfL as a calibrator. Calibrators were  
51 run as triplicates, while plasma samples were measured in singlicate. All the available samples  
52 were analyzed in a single batch.  
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## MRI–score for A $\beta$ -positivity

3T multimodality MRI data included a 3D MP-RAGE or IR-SPGR T1-weighted MRI with sagittal slices and voxel size of  $1\times 1\times 1\text{mm}^3$ , as described online (<http://adni.loni.usc.edu/methods/documents/mri-protocols>). We employed a previously proposed methodology for assessing brain A $\beta$  positivity status (Lang *et al.*, 2019). Briefly, 972 ADNI subjects with structural MRI scans and with known A $\beta$  status based on either CSF or A $\beta$  PET imaging were used to train a deep learning (DL) model. The DL model training cohort included individuals at different clinical stages (CU, subjective memory complaint, early/late MCI, and dementia), but excluding the subjects of the current study with plasma biomarker data. The method yields a probabilistic score of A $\beta$ -positivity between 0 and 1.

## Statistical analysis

All analyses were performed on CU and CI data separately.

Demographic, clinical, and biomarker characteristics differences between A $\beta$ + and A $\beta$ - participants were described using two-sample *t*-test and the  $\chi^2$  test for continuous and categorical variables, respectively.

Demographic characteristics (age, sex, years of education), *APOE* genotype, cognitive scores (MMSE, ADAS–Cog, and CDR–SB), plasma A $\beta_{42}$ /A $\beta_{40}$ , p-tau181, and NfL levels, and derived MRI–score were used as inputs to construct random forest (RF) classifiers to detect the A $\beta$ -positivity using florbetapir PET status as the ground-truth. Random forest approach was pre-selected based on classification performances previously reported (Delgado *et al.*, 2014) and flexibility of RF models to a mixture of numerical (age, years of education, cognitive scores, plasma levels, and MRI–score) and categorical (sex and *APOE* genotype) features. A reference RF classifier was constructed from demographics and cognitive scores, referred as the clinical information here on. A second reference RF classifier was also constructed from MRI–score alone. To assess the added value of each class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical features, 3) MRI–score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI–score.

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3 The random forest model construction was repeated 10 times using different random seeds, and  
4 the average model performance was reported. Each dataset (CU and CI datasets) was randomly  
5 divided into training and test datasets, using non-overlapping 80%/20% split. Each dataset used  
6 the same partitioning for all classifiers for an unbiased comparison between classifiers  
7 (Vanschoren *et al.*, 2012). The models were built on each training split, and the performance on  
8 the test datasets were evaluated, and this process was repeated 10 times. Performance was  
9 presented as mean and standard deviation over the model runs. We generated sensitivity-  
10 specificity curves based on model classifications on the test data. For each sensitivity-specificity  
11 curve, we also computed the area under curve (AUC) values. A confidence interval of 95% was  
12 chosen. AUC of two classifiers were compared with DeLong test (DeLong *et al.*, 1988).  
13 Additionally, we computed accuracy, sensitivity, specificity, positive predictive value (PPV),  
14 and negative predictive value (NPV) on each set of model classifications at classifier probability  
15 cut-off of 0.5.  
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27 Finally, for random forest models with multiple variables the mean decrease in accuracy a  
28 variable caused was determined based on the out of bag error estimates. The more the accuracy  
29 of the random forest decreases due to the exclusion of a single variable, the more important that  
30 variable was deemed for classification of the data.  
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35 The main analyses reported below with PET A $\beta$ -positivity as the gold-standard for A $\beta$ -positivity  
36 were repeated with CSF A $\beta$ -positivity and results were provided in Supplementary Figure 1.  
37 Results from another secondary analysis were also provided in Supplementary Figure 2, where  
38 each classifier model was considered in a sub-sample constraint by the plasma A $\beta_{42}$ /A $\beta_{40}$  cohort  
39 where all relevant data was available, therefore a fixed sample size across all classifier models  
40 considered in this study. Finally, the main analyses were repeated by restricting clinical  
41 information to age and *APOE* genotype, as reported in Supplementary Figure 3.  
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48 All analyses were done using the R language and environment for statistical computing version  
49 4.0.1 (R Foundation for Statistical Computing).  
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### 53 **Data availability**

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3 Data used in this study has been made publicly available by the ADNI in the Laboratory of  
4 Neuro Imaging (LONI) database.  
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## 7 8 **Results** 9

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11 Plasma  $A\beta_{42}/A\beta_{40}$  results for nine CU and nine CI participants failed quality control at  
12 measurement. No outliers (i.e.,  $> 4$  standard deviations of the mean) were detected in the plasma  
13  $A\beta_{42}/A\beta_{40}$  measurements. Samples from three CU and one CI participants were measured below  
14 the lower limit of quantification of 1.0 pg/mL for plasma p-tau181. We identified additional five  
15 CU and five CI participants with outlier values of plasma p-tau181 levels that were discarded from  
16 subsequent analyses. Analytical sensitivity for plasma NfL was  $<1.0$  pg/mL, and no sample  
17 contained NfL levels in plasma below the limit of detection, but five CUs and 11 CIs were excluded  
18 from our analyses due to outlier plasma NfL values. Participants with dementia were excluded for  
19 two main reasons. First, 91% of the AD participants ( $n=235$ ) with plasma NfL and plasma p-  
20 tau181 biomarker data were PET  $A\beta$ -positive. An unbiased classification performance analysis  
21 with a prevalence of 91%  $A\beta$ -positivity would have required a sample size greater than 500  
22 (Hanczar *et al.*, 2010). Second, cross-sectional plasma  $A\beta_{42}/A\beta_{40}$  data was only available for  
23 undemented participants. The final main study cohort was composed of 333 CU and 519 CI elderly  
24 individuals. Participant characteristics are reported in Table 1.  
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37 Thirty-three percent of CU participants in the main study cohort were PET  $A\beta^+$ . The frequency of  
38 *APOE*  $\epsilon 4$  allele was higher among  $A\beta^+$  CUs compared to  $A\beta^-$  CUs. Compared to  $A\beta^-$  CUs,  $A\beta^+$   
39 CUs were older with fewer females and had significantly fewer years of education, greater CDR-  
40 SB and ADAS-Cog scores, as well as greater plasma NfL levels (Figure 1). Plasma p-tau181 levels  
41 were marginally higher in  $A\beta^+$  CUs compared to  $A\beta^-$  CUs ( $p=0.057$ ). When controlled for age  
42 differences,  $A\beta^-$  CUs and  $A\beta^+$  CUs did not differ in ADAS-Cog scores and plasma NfL levels.  
43 Demographic and clinical characteristics of CUs in the plasma  $A\beta_{42}/A\beta_{40}$  sub-cohort did not differ  
44 from those of the main study CUs. Within the plasma  $A\beta_{42}/A\beta_{40}$  sub-cohort,  $A\beta^+$  CUs had lower  
45 plasma  $A\beta_{42}/A\beta_{40}$  compared to  $A\beta^-$  CUs (Figure 1;  $p<10^{-6}$ ).  
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54 Fifty-seven percent of CI participants in the main study cohort were PET  $A\beta^+$ .  $A\beta^+$  CIs were older  
55 than  $A\beta^-$  CIs with fewer years of education and a higher frequency of *APOE*  $\epsilon 4$  allele. Compared  
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3 to A $\beta$ - CIs, A $\beta$ + CIs had greater clinical symptoms, with lower MMSE and higher CDR-SB and  
4 ADAS-Cog scores. A $\beta$ + CIs had significantly higher plasma p-tau181 and plasma NfL levels than  
5 A $\beta$ - CIs (Figure 1). A $\beta$ - vs A $\beta$ + CI group differences in clinical scores and plasma levels were  
6 significant after controlling for age differences. Compared to the CIs in the main study cohort, CIs  
7 in the plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> sub-cohort had lower symptom severity (i.e., mean CDR-SB of 1.4 vs  
8 0.7 with  $p < 10^{-15}$  and mean ADAS-Cog of 9.2 vs 7.8 with  $p=0.002$ ) and lower plasma NfL levels  
9 (39.5pg/ml vs 34.5pg/ml with  $p=0.01$ ). Within the plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> sub-cohort, A $\beta$ + CIs had  
10 significantly lower plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> compared to A $\beta$ - CIs (Figure 1;  $p < 10^{-10}$ ).  
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### 18 **Differentiating A $\beta$ + and A $\beta$ - CU participants, Figures 2a-3a (Supp Figure 4) and Table 2.**

19 A classifier constructed with only clinical information (i.e., demographics, *APOE*  $\epsilon$ 4 carrier  
20 status, and global cognitive assessments) and a classifier constructed with only the MRI-score  
21 had similar performances (i.e., DeLong  $p=0.06$ ) with an accuracy of 67-68% in differentiating  
22 A $\beta$ + CUs and A $\beta$ - CUs. Of these two classifiers, the MRI-score yielded better AUC (0.74 vs  
23 0.69) reflected in higher NPV of MRI-score (76% vs 68%) and poor sensitivity of clinical  
24 information (3% vs 46%). When considered alone and together, plasma p-tau181 and plasma  
25 NfL did not differentiate A $\beta$ + and A $\beta$ - CUs better than chance (Table 2; column (A)). In  
26 contrast, plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> alone differentiated A $\beta$ + CUs from A $\beta$ - CUs with an accuracy of  
27 72%, a PPV of 69%, and an NPV of 76%, yielding an AUC of 0.80. The overall performance of  
28 plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> only classifier was similar to the performance of a classifier using MRI score  
29 and clinical information jointly (i.e., AUC of 0.80; DeLong  $p=0.53$ ), with plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub>  
30 having slightly better PPV (69% vs 65%) whereas the multidisciplinary MRI score and clinical  
31 information jointly having slightly better accuracy (i.e., 75% vs 72%) and NPV (i.e., 78% vs  
32 76%). All three plasma biomarkers jointly differentiated A $\beta$ + CU and A $\beta$ - CU at an improved  
33 accuracy of 77%, a PPV of 77% and an NPV of 80%, yielding an AUC of 0.83, but this was not  
34 significantly different than the performance of plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> alone classification (DeLong  
35  $p=0.09$ ).  
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51 When combined with clinical information (Table 2; column (B)), the predictive performance of  
52 the plasma p-tau181 and plasma NfL improved but not beyond the performance of the classifier  
53 constructed from clinical information alone (i.e., DeLong  $p=0.18$  and  $p=0.08$ , respectively).  
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3 Adding clinical information to the plasma  $A\beta_{42}/A\beta_{40}$  classifier yielded better differentiation of  
4  $A\beta+$  CU and  $A\beta-$  CU cases with an accuracy of 79%, PPV of 77%, NPV of 81%, and an AUC  
5 0.86, with the greatest improvement in the PPV compared to plasma  $A\beta_{42}/A\beta_{40}$  only and clinical  
6 information only classifiers. Further enhancing plasma NfL and plasma p-tau181 with the MRI  
7 score in addition to the clinical information improved classification accuracy by 5%–8%, PPV by  
8 13%–22%, NPV by 8%–11%, and AUC by 0.10 to 0.14 (DeLong  $p < 10^{-14}$  and  $p < 10^{-21}$ ,  
9 respectively) but this was not better than the classifier constructed with the MRI–score and  
10 clinical information (i.e., DeLong  $p = 0.08$  and  $p = 0.46$ , respectively) or the classifier based on  
11 plasma  $A\beta_{42}/A\beta_{40}$  only (i.e., DeLong  $p = 0.07$  and  $p = 0.88$ , respectively), as reported in Table 2;  
12 column (C). Of the three plasma biomarkers,  $A\beta_{42}/A\beta_{40}$  in combination with the MRI–score and  
13 clinical information performed the best with an accuracy of 83% and AUC of 0.90, with a well-  
14 balanced PPV of 84% and NPV of 83%, which was significantly better than the performance of  
15  $A\beta_{42}/A\beta_{40}$  alone (i.e., DeLong  $p < 10^{-4}$ ) or in combination with clinical information (i.e., DeLong  
16  $p = 0.02$ ).

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19 The full classifier model including all three plasma biomarkers, the MRI–score, and clinical  
20 information had an accuracy of 82%, with a PPV of 90% and NPV of 79%. However, this was  
21 not significantly different from the classifier model with plasma  $A\beta_{42}/A\beta_{40}$ , MRI–score, and  
22 clinical information (DeLong  $p = 0.61$ ), suggesting minimal added value of plasma NfL and  
23 plasma p-tau181. The most significant variables in a decreasing order of importance based on  
24 mean decrease in accuracy analysis were plasma  $A\beta_{42}/A\beta_{40}$ , MRI–score, *APOE*  $\epsilon 4$  status,  
25 MMSE, years of education, and sex.

### 26 27 28 **Differentiating $A\beta+$ and $A\beta-$ CI participants, Figures 2b-3b (Supp Figure 4) and Table 3.**

29 Both clinical information-based and MRI–score-based classifiers performed moderately well in  
30 differentiating  $A\beta+$  and  $A\beta-$  CIs with an AUC of 0.81 and 0.76, accuracy of 74% and 67%, PPV  
31 of 76% and 70%, and NPV of 73% and 63%, respectively. The MRI–score together with clinical  
32 information achieved an AUC of 0.88, with an accuracy of 81%, PPV of 82%, and NPV of 80%,  
33 performing significantly better than clinical information only (DeLong  $p < 10^{-15}$ ) or MRI–score  
34 only (DeLong  $p < 10^{-39}$ ) models. In contrast to CU data, both plasma  $A\beta_{42}/A\beta_{40}$  and plasma p-  
35 tau181, but not plasma NfL, separately detected  $A\beta$ -positivity in CIs with an average accuracy of  
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77% and 58%, PPV of 79% and 63%, NPV of 76% and 52%, yielding AUCs of 0.87 and 0.64, respectively. Enhancement with clinical information improved performance metrics of plasma p-tau181 and NfL, but not plasma  $A\beta_{42}/A\beta_{40}$ , classifiers by 15 to 23% (Table 3; column (B)). Plasma p-tau181 enhanced with clinical information perform similarly to plasma  $A\beta_{42}/A\beta_{40}$ . When further enhanced with the MRI-score in addition to the clinical information, classifier performance metrics for both plasma p-tau181 and plasma NfL increased by an additional 3 to 8%, with plasma p-tau181 performing slightly better with an accuracy of 82%, PPV of 83% PPV, and NPV of 82% (Table 3; column (C)). Similarly, the MRI-score enhanced classification performance of plasma  $A\beta_{42}/A\beta_{40}$  more than clinical information (DeLong  $p < 10^{-4}$ ), reaching an AUC of 0.94 with an accuracy of 86%, PPV of 86%, and NPV of 88%. The full classifier model, including all three plasma biomarkers, MRI-score, and clinical information achieved an AUC of 0.92 and an accuracy of 86%, with a PPV of 88% and NPV of 86%. This was not significantly different than the classifier model with plasma  $A\beta_{42}/A\beta_{40}$ , MRI-score, and clinical information (DeLong  $p = 0.31$ ), suggesting minimal added value of plasma NfL and plasma p-tau181. The most significant variables in a decreasing order of importance based on mean decrease in accuracy analysis were plasma  $A\beta_{42}/A\beta_{40}$ , MRI-score, *APOE*  $\epsilon 4$  allele, age, and CDR-SB.

## Discussion

The major findings of this multicenter biomarker study were (1) of the three plasma biomarkers, when considered separately,  $A\beta_{42}/A\beta_{40}$  consistently differentiated PET  $A\beta$ -positivity status both in CU and CI participants, with a slightly better performance in CIs, whereas plasma p-tau181 showed moderate value for differentiating PET  $A\beta$ -positivity status in CI participants, and plasma NfL lacked  $A\beta$ -positivity stratification value both in CU and CI participants; (2) clinical information, dominated by *APOE*  $\epsilon 4$  status and education in CU participants, and by *APOE*  $\epsilon 4$  status and age in CI participants, as well as MRI-score independently differentiated PET  $A\beta$ - and  $A\beta^+$  both in CU and CI participants; (3) clinical information enhanced performance of plasma biomarkers in differentiating PET  $A\beta$ - and  $A\beta^+$  participants by 0.06 to 0.14 units of AUC for CUs, and by 0.21 to 0.25 units for CIs; and (4) further enhancement of these models with an MRI-score yielded an additional improvement of 0.04 to 0.11 units of AUC for CUs and 0.05 to 0.09 units for CIs. Taken together the results recapitulate plasma  $A\beta_{42}/A\beta_{40}$  as a robust

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3 biomarker of brain A $\beta$ -positivity and suggest that when combined with clinical information,  
4 plasma p-tau181 and NfL biomarkers, and an MRI-score, could effectively identify A $\beta$ +  
5 individuals with expected greater accuracy in the symptomatic individuals. Interestingly, when  
6 the MRI-score is considered in combination with clinical information, plasma p-tau181 and  
7 plasma NfL have minimal added value for brain A $\beta$ -positivity stratification in this multicenter  
8 ADNI cohort of CU and CI participants.  
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15 Plasma A $\beta_{42}$ /A $\beta_{40}$  detects PET A $\beta$ -positivity. The first major finding was that plasma A $\beta_{42}$ /A $\beta_{40}$   
16 was a robust biomarker of PET A $\beta$ -positivity independent of clinical diagnosis, whereas plasma  
17 p-tau181 detected PET A $\beta$ -positivity only in CIs with a moderate accuracy, and plasma NfL  
18 lacked value for stratification of PET A $\beta$ + and PET A $\beta$ - cases both in CU and CI cohorts. It  
19 should be noted that this finding was replicated when the modeling and testing of all classifiers  
20 were repeated on the plasma A $\beta_{42}$ /A $\beta_{40}$  sub-cohort to mitigate the potential influence of sample  
21 size and sub-cohort characteristics in comparisons of classifiers (Supplementary Figure 2). Of  
22 the three plasma biomarkers considered in this study, A $\beta_{42}$ /A $\beta_{40}$  has been the most extensively  
23 studied in the literature. Recent studies, particularly the ones using highly sensitive mass  
24 spectrometry, have repeatedly reported a strong correlation between plasma A $\beta_{42}$ /A $\beta_{40}$  and the  
25 gold-standard CSF and PET A $\beta$  measures (Janelidze *et al.*, 2016; Ovod *et al.*, 2017b; Nakamura  
26 *et al.*, 2018; Schindler *et al.*, 2019). Consistent with our findings, plasma A $\beta_{42}$ /A $\beta_{40}$ , especially  
27 when combined with age and *APOE*  $\epsilon$ 4 status, have been shown to accurately stratify A $\beta$ +  
28 individuals (e.g., AUC of 0.80-0.85) in the AD continuum (Palmqvist *et al.*, 2019b; Schindler *et*  
29 *al.*, 2019). The slightly superior performance of plasma A $\beta_{42}$ /A $\beta_{40}$  in this study (cf.  
30 Supplementary Figure 3) compared to previous reports of 0.79-0.82 AUC for the detection of  
31 A $\beta$ -positivity in CU participants (Fandos *et al.*, 2017; de Rojas *et al.*, 2018; Chatterjee *et al.*,  
32 2019) and 0.90 AUC for CIs (Lin *et al.*, 2019) might be due to high molecular specificity and  
33 detection sensitivity of LC-MS/MS technique used to analyze the ADNI plasma samples. This  
34 observation is consistent with the notion that the different assays for plasma A $\beta_{42}$ /A $\beta_{40}$  may have  
35 different precision and, in particular, mass spectrometry-based assays compared to  
36 immunoassays might be more accurate and robust in measuring levels of plasma A $\beta$  species as  
37 biomarker of brain A $\beta$  (Zetterberg, 2019). Another factor contributing to the high performance  
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3 of the  $A\beta_{42}/A\beta_{40}$  ratio, as compared with single biomarkers, is that between-individual  
4 differences in basal “total”  $A\beta$  secretion is compensated for in the ratio, by dividing with  $A\beta_{40}$ ,  
5 while such differences in plasma NfL and p-tau181 levels, MRI measures, or cognitive abilities  
6 might introduce variability in these measures.  
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11 Plasma p-tau181 presented a more complex picture as a candidate biomarker of brain  $A\beta$ -  
12 positivity. Assays for the quantification of plasma p-tau181 are very recently developed  
13 (Zetterberg and Blennow, 2020) and are still under extensive investigation to fully understand  
14 the role of different plasma tau species as peripheral markers of AD pathophysiology. Compared  
15 to the limited number of previously reported evaluations of plasma p-tau181 as a biomarker of  
16 brain  $A\beta$ -positivity in other research and clinical cohorts (Mielke *et al.*, 2018; Palmqvist *et al.*,  
17 2019b; Barthélemy *et al.*, 2020; Janelidze *et al.*, 2020a; Karikari *et al.*, 2020; Thijssen *et al.*,  
18 2020), ADNI plasma p-tau181 levels measured by the Simoa assay differentiated between PET  
19  $A\beta+$  and PET  $A\beta-$  ADNI CI participants with an inferior accuracy (AUC of 0.64). Furthermore,  
20 this biomarker had no stratification value for PET  $A\beta$ -positivity within the ADNI CU  
21 participants (AUC of 0.55). The addition of clinical information to this base model increased  
22 AUC for the classification of  $A\beta+$  vs  $A\beta-$  by 0.14 to 0.69 in CUs and by 0.21 to 0.85 in CIs. The  
23 subsequent addition of an MRI-score to this model further increased AUC for the classification  
24 of  $A\beta+$  vs  $A\beta-$  by 0.11 to 0.80 in CUs and by 0.05 to 0.90 in CIs, bringing its classification  
25 performance to a clinically acceptable level.  
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39 Potential sources of the discrepancy between our results and those of other groups may include  
40 differences in the plasma analysis assays, diagnostic composition and demographic  
41 characteristics of the study cohorts, methodology used to determine ground-truth brain  $A\beta$ -  
42 positivity status, and data analytics. One of the earliest plasma p-tau181 studies on a Meso Scale  
43 Discovery (MSD) platform reported that plasma p-tau181 as a good biomarker of the elevated  
44 brain  $A\beta$  with an AUC of 0.7 in CU and 0.85 in MCI participants in their discovery cohort but  
45 this study lacked internal validation or replication in an external validation cohort (Mielke *et al.*,  
46 2018). Another study (Barthélemy *et al.*, 2020) reported high specificity of plasma p-tau181,  
47 measured by a highly sensitive mass spectrometry assay, for  $A\beta$  plaque pathology in their  
48 discovery cohort ( $n=34$ ; including clinically diagnosed CU, MCI, and AD individuals) and then  
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3 replicated their findings with an AUC of 0.72 to differentiate A $\beta$ <sup>-</sup> and A $\beta$ <sup>+</sup> individuals in an  
4 independent replication cohort of CUs, MCIs, and ADs ( $n=92$ ) but the performance within CU  
5 only or MCI only sub-cohorts was not statistically significant. Similarly, a larger multi-cohort  
6 study which included individuals with various clinical diagnoses including CU, MCI, and AD  
7 reported a stepwise increase in plasma p-tau181 levels, measured on the MSD platform, with  
8 both A $\beta$ -positivity and cognitive impairment and achieved an AUC of 0.81 in differentiating  
9 A $\beta$ <sup>-</sup> and A $\beta$ <sup>+</sup> individuals, which was increased to 0.84 with the addition of plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub>  
10 (Janelidze *et al.*, 2020a).  
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18 The age of cohort participants may also influence the ability of plasma p-tau181 to detect A $\beta$ -  
19 positivity status. For instance, a multi-cohort study used the Simoa assay to measure plasma p-  
20 tau181 in four different cohorts (Karikari *et al.*, 2020) and found that plasma p-tau181 biomarker  
21 discriminated A $\beta$ <sup>+</sup> CU older adults and individuals with CI from A $\beta$ <sup>-</sup> CU older adults and young  
22 adults with an AUC of 0.76–0.88 across cohorts. However, the CU older adults in this study  
23 were on average 10 years younger than ADNI participants, raising the question about age-  
24 dependent sensitivity of plasma p-tau181 to AD-related A $\beta$  pathology. Similarly, another small  
25 cohort study of CU and CI participants, who were on average 13 years younger than ADNI  
26 participants, reported an excellent AUC of 0.86 in CU and 0.94, although not internally validated  
27 or replicated in an external cohort, in differentiating PET A $\beta$ <sup>+</sup> and PET A $\beta$ <sup>-</sup> CIs with plasma p-  
28 tau181 levels (Thijssen *et al.*, 2020). It is highly likely that younger A $\beta$ <sup>+</sup> participants might have  
29 greater pathophysiological changes than the older ADNI participants in response to A $\beta$  toxicity,  
30 which might be a driving factor for increased plasma p-tau181 levels. Indeed, it is well  
31 established that younger individuals who are A $\beta$ <sup>+</sup> have more brain tau deposition than older  
32 individuals who are A $\beta$ <sup>+</sup> (Schöll *et al.*, 2017). Furthermore, previous studies found that the  
33 strong correlations between plasma p-tau181 and A $\beta$  PET are often in the A $\beta$ <sup>+</sup> but not in A $\beta$ <sup>-</sup>  
34 individuals (Janelidze *et al.*, 2020a) and that increased plasma p-tau181 levels might be initiated  
35 by accumulation of A $\beta$  beyond the positivity threshold, and continue to increase as A $\beta$  further  
36 accumulates in the brain even during early stages of tau pathology as measured by Braak &  
37 Braak staging at autopsy or tau PET during life (Janelidze *et al.*, 2020a; Karikari *et al.*, 2020).  
38 Evidence from these recent studies together with the stronger association of plasma p-tau181  
39 with brain A $\beta$  burden in younger cohorts might suggest that plasma p-tau181 is unlikely to be a  
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3 direct measure of A $\beta$  pathology but instead a marker of tau pathology. Our finding that plasma p-  
4 tau181 has moderate stratification accuracy for PET A $\beta$ -positivity only at the symptomatic  
5 disease stage suggests that p-tau181 detects A $\beta$ -positivity only once a significant tau pathology,  
6 which is closely associated with symptoms, is detectable.  
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11 Plasma NfL was a poor biomarker of PET A $\beta$ -positivity: The relatively poor performance of  
12 plasma NfL in differentiating A $\beta$ + and A $\beta$ - ADNI individuals, either symptomatic or  
13 asymptomatic, is largely consistent with previous literature. Previous studies found no evidence  
14 that plasma NfL was related to A $\beta$  or tau pathology as measured by PET or even synaptic  
15 dysfunction as measured by fluorodeoxyglucose (FDG)-PET imaging, repeatedly emphasizing  
16 that plasma NfL is more likely to be a marker of all cause neurodegeneration (Mattsson *et al.*,  
17 2019; Mielke *et al.*, 2019; Janelidze *et al.*, 2020a; Thijssen *et al.*, 2020). Finally, our finding that  
18 plasma p-tau181 and plasma NfL did not improve A $\beta$ -positivity stratification accuracy above  
19 and beyond the plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> was consistent with previous studies on other AD research  
20 cohorts (Palmqvist *et al.*, 2019b).  
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30 Clinical information and MRI-score independently differentiated PET A $\beta$ + and A $\beta$ - ADNI  
31 individuals: To date, the most common candidate predictors considered for A $\beta$ -positivity were  
32 age, *APOE* genotype, and measures of cognition, largely because they are easier to collect with  
33 widely available standardized protocols. Of these, age has been the most common predictor of  
34 elevated brain A $\beta$  followed by the *APOE* genotype (reviewed in (Ashford *et al.*, 2020)),  
35 consistent with the notion that after advanced age, *APOE*  $\epsilon$ 4 genotype is a major risk factor for  
36 developing AD (Payami *et al.*, 1997). Consistent with the prior knowledge, age and *APOE*  
37 genotype were important predictors of A $\beta$ -positivity for ADNI CU and CI participants (cf.  
38 Supplementary Figure 3). In the main analyses, we observed that the ability of clinical  
39 information to differentiate A $\beta$ + and A $\beta$ - participants improved, especially in terms of  
40 sensitivity, with increasing severity of clinical diagnosis. Indeed, measures of global cognition,  
41 such as MMSE and CDR-SB, had greater influence in the classifier model for A $\beta$ -positivity  
42 within the CI participants. Consistent with our findings, accumulating evidence suggests that  
43 elevated A $\beta$  is associated with risk of cognitive worsening and may indicate a pre-symptomatic  
44 stage of disease (Roe *et al.*, 2013; Donohue *et al.*, 2017). As the relationships between cognition  
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3 and AD biomarkers are expected to be subtle, the global measures of cognition may have  
4 insufficient sensitivity among CUs to reliably detect pre-symptomatic expression of A $\beta$   
5 pathology, as reflected in our results with extremely low sensitivity of clinical information in  
6 detecting A $\beta$ -positivity in CUs.  
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11 MRI-score of brain A $\beta$  alone stratified A $\beta$ + and A $\beta$ - participants with an AUC of 0.74 in ADNI  
12 CUs and an AUC of 0.76 in ADNI CIs with a substantially increased sensitivity. When  
13 combined with clinical information, MRI-score performed as well as, or, in CIs, even better  
14 than, the best performing plasma biomarker, A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub>. Although structural T1-weighted MRI is  
15 not a molecular imaging modality directly targeting quantification of protein accumulation in the  
16 brain, MRI has been a gold standard for neurodegeneration (Jack *et al.*, 2004). The evidence for  
17 a relationship between A $\beta$  deposition and neurodegeneration has been previously demonstrated  
18 in very early AD and even in asymptomatic individuals (Bourgeat *et al.*, 2010; Chételat *et al.*,  
19 2010). In a similar manner to plasma p-tau181, the value of the MRI-score for A $\beta$ -positivity  
20 might be a reflection of neurodegenerative processes due to A $\beta$  toxicity, yet we observed that the  
21 MRI-score outperformed the plasma p-tau181. The brain A $\beta$  deposition has a spatially distinct  
22 signature of cortical atrophy (Bourgeat *et al.*, 2010; Chételat *et al.*, 2010; Tosun *et al.*, 2011) and  
23 MRI-based correlates of brain A $\beta$  deposition compared to plasma analytes might have the  
24 advantage of capturing this spatial information. Furthermore, although structural T1-weighted  
25 imaging has been traditionally considered to reveal fat and water distribution and distinguish  
26 tissue types, cellular changes associated with neuropathology might also influence the MRI  
27 contrast as well as the MRI intensity quality, such as the gray value distribution, texture features,  
28 and spatial heterogeneity (Sørensen *et al.*, 2016; Feng *et al.*, 2019; Ranjbar *et al.*, 2019). Our  
29 results also suggest that deep learning, the computational approach used in this study to construct  
30 MRI-scores, might efficiently quantify A $\beta$  toxicity from structural MRI because of its high  
31 automatic feature learning and visual pattern recognition abilities (LeCun *et al.*, 2015).  
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50 Both clinical information and MRI-score enhanced performance of plasma biomarkers in  
51 identifying PET A $\beta$ -positivity. One interesting observation was that although when combined  
52 with clinical information and MRI-score, plasma p-tau181 and NfL biomarkers could effectively  
53 identify A $\beta$ + symptomatic individuals, plasma p-tau181 and plasma NfL did not contribute to the  
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3 detection of brain A $\beta$  above and beyond the classification power of clinical information and  
4 MRI-score jointly, particularly in CUs. This is a particularly important criterion in the selection  
5 of candidate cost-effective and rapid screening tools for broad implementation in clinical and  
6 drug trial settings. Demographics and global cognitive measures are an integral part of the  
7 clinical assessment. MRI has long played a role in inclusion and exclusion criteria in patient  
8 recruitment and ruling out other causes of cognitive symptoms (Frisoni *et al.*, 2010).

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10 Furthermore, MRI has been routinely acquired in clinical trials to identify and monitor adverse  
11 events (Cash *et al.*, 2014). Plasma biomarkers, therefore, should have a classification ability as  
12 good as or better than clinical information and MRI separately and in combination in order to be  
13 a practical non-invasive screener.  
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16 Our results in this ADNI study, although limited to CU and CI participants, suggest that plasma  
17 A $\beta_{42}$ /A $\beta_{40}$  but not plasma p-tau181 and plasma NfL might have added value in screening for  
18 brain A $\beta$ -positivity. It is also important to emphasize that plasma assays target brain-derived  
19 proteins that are present at extremely low concentrations in the peripheral circulation and  
20 originate not only in the brain but almost all peripheral cells (Roher *et al.*, 2009). What plasma  
21 A $\beta$  measures mean biologically and to what extent the variances seen in plasma A $\beta$  levels reflect  
22 brain pathology especially in the CU and CI clinical groups in which greater heterogeneity in  
23 comorbid conditions is expected are questions still warrant further investigations. These  
24 limitations may make the use of the plasma A $\beta$  biomarkers to predict the AD pathology more  
25 difficult at the individual level. Despite the inferior performance of plasma p-tau181 in detecting  
26 AD A $\beta$ -positivity observed in this ADNI cohort, this biomarker may have different utility.  
27 Plasma p-tau181 can be robustly measured in plasma and is highly specific for AD pathology  
28 (Mielke *et al.*, 2018), making it an attractive screening tool for brain A $\beta$  and tau pathologies  
29 jointly as required for A/T/N biomarker profiling (Jack *et al.*, 2018) linked to differential  
30 trajectories of disease progression (Altomare *et al.*, 2019; Jack *et al.*, 2019; Ebenau *et al.*, 2020).  
31 Further studies are warranted to better understand the behavior of plasma p-tau181 as a  
32 biomarker of the burden of the disease at different disease stages (Lantero Rodriguez *et al.*,  
33 2020). Given that A $\beta$ -positivity assessment using either CSF or PET is independent of clinical  
34 diagnosis, clinical stage dependent classifier performance might be a concern if these plasma  
35 biomarkers are operationalized in clinical practice. In our analysis, a similar clinical diagnosis-

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3 dependent gradual increase in classification performance was observed in A $\beta$ -positivity classifier  
4 constructed with clinical information and to a lesser extent with MRI-score.  
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### 8 **Study design-specific considerations**

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11 There are multiple strengths to the study including the large sample size, well-characterized  
12 participants, and availability of plasma analytes, A $\beta$  PET imaging, and structural MRI, all  
13 assessed within a short period of time. A limitation of this *in vivo* study was the use of A $\beta$  PET  
14 as the gold standard for brain A $\beta$ -positivity rather than the true gold standard of neuropathology.  
15 A limitation of plasma analyte comparisons is that different techniques were used, namely Simoa  
16 for p-tau181 and NfL and LC-MS/MS for A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub>. Despite the superior specificity, mass  
17 spectrometry has the disadvantage of being more expensive and requiring more expertise than  
18 immunoassays, which are easily analyzed by laboratories that routinely run blood tests. Another  
19 limitation of the study is the potential pre-analytical variability since the blood samples were  
20 collected at multiple ADNI sites. Although the collection site as a categorical variable had no  
21 significant effect on ADNI plasma levels, multicentre studies of plasma analytes still require  
22 further investigation for standardization of protocols to reduce measurement variability (Rozga *et*  
23 *al.*, 2019). We should also note that the current study was limited to plasma p-tau181. Other  
24 blood immunoassays targeting tau species, specifically the very recently reported plasma pTau-  
25 217, might be promising biomarkers for AD A $\beta$  pathology (Janelidze *et al.*, 2020b). Finally, we  
26 should further emphasize that the current study is based on a convenience cohort where the  
27 degree of true population representation is not known. Most notable, about 47% of CU and 19%  
28 of CI ADNI participants who were CSF p-tau positive were PET A $\beta$ <sup>-</sup>, suggesting non-AD  
29 etiology of their tau pathology that might have particularly impacted the observed plasma p-  
30 tau181 levels (Benussi *et al.*, 2020). Additionally, the PPV and NPV performance of the  
31 classifier models considered in this study were limited by the prevalence of the PET A $\beta$ -  
32 positivity in the selected ADNI cohort and may not be directly comparable to other studies with  
33 different PET A $\beta$ -positivity prevalence.  
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### 51 **Conclusion**

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3 In summary, *in vivo* gold standard for brain A $\beta$  burden assessment is currently A $\beta$  PET or  
4 lumbar puncture for CSF A $\beta_{42}$  (Tapiola *et al.*, 2009; Palmqvist *et al.*, 2016). The widespread  
5 acceptance of biomarker classification scheme for the AD continuum (Jack *et al.*, 2018) has  
6 ignited interest in more affordable and accessible approaches to detect AD A $\beta$  pathology, a  
7 process that often slows down the recruitment into, and adds to the cost of, clinical trials. To this  
8 end, our systematic comparison of A $\beta$ -positivity stratification models that use minimally  
9 invasive and low-cost measures identified demographics, *APOE* genotype, global cognitive  
10 measures, MR imaging, plasma A $\beta$  measures, plasma p-tau181, and plasma NfL biomarkers,  
11 some alone and some in combination, as promising A $\beta$ -positivity classifiers. Advances in  
12 ultrasensitive assays for plasma analytes as well as in computational classifier techniques  
13 combining multidisciplinary information further promise reduce the difficulty and cost of  
14 screening participants with AD A $\beta$  pathology.  
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## 31 **Conflicts of interest**

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33  
34 Dr. Jack serves on an independent data monitoring board for Roche, has consulted for and served  
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11 Dr. Zetterberg has served at scientific advisory boards for Denali, Roche Diagnostics, Wave,  
12 Samumed, Siemens Healthineers, Pinteon Therapeutics and CogRx, has given lectures in symposia  
13 sponsored by Fujirebio, Alzecure and Biogen, and is a co-founder of Brain Biomarker Solutions  
14 in Gothenburg AB (BBS), which is a part of the GU Ventures Incubator Program.  
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19 Dr. Blennow has served as a consultant, at advisory boards, or at data monitoring committees for  
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21 Diagnostics, and Siemens Healthineers, and is a co-founder of Brain Biomarker Solutions in  
22 Gothenburg AB (BBS), which is a part of the GU Ventures Incubator Program.  
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27 Dr. Bateman cofounded C2NDiagnostics. Washington University and RJB have equity ownership  
28 interest in C2N Diagnostics and receive royalty income based on technology (stable isotope  
29 labeling kinetics and blood plasma assay) licensed by Washington University to C2N Diagnostics.  
30 Dr. Bateman receives income from C2N Diagnostics for serving on the scientific advisory board.  
31 Washington University, with Dr. Bateman as coinventor, has submitted the US provisional patent  
32 application "Plasma Based Methods for Detecting CNS Amyloid Deposition." Dr. Bateman  
33 consults for Roche, Genentech, AbbVie, Pfizer, Boehringer-Ingelheim, and Merck.  
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### Figure Captions:

Figure 1. Plasma a)  $A\beta_{42}/A\beta_{40}$ , b) NfL concentrations, and c) p-tau181 concentrations categorized by clinical diagnosis and CSF  $A\beta$ -positivity. Plasma  $A\beta_{42}/A\beta_{40}$  data was available for 173 individuals ( $A\beta^-$  CU,  $n=50$ ;  $A\beta^+$  CU,  $n=37$ ;  $A\beta^-$  CI,  $n=40$ ;  $A\beta^+$  CI,  $n=46$ ). Plasma p-tau181 and NfL data included 852 individuals ( $A\beta^-$  CU,  $n=224$ ;  $A\beta^+$  CU,  $n=109$ ;  $A\beta^-$  CI,  $n=230$ ;  $A\beta^+$  CI,  $n=289$ ). Unpaired two-samples t-test uncorrected significance levels at \*\*\*\*:  $p < 0.00001$ ; \*\*\*:  $p < 0.0001$ ; \*\*:  $p < 0.001$ ; ns:  $p \geq 0.5$ . CU: Cognitively unimpaired elderly; CI: Elderly individuals with mild cognitive impairment.

Figure 2. Receiver operating characteristic (ROC) analysis of  $A\beta$  positivity prediction in an ADNI cohort of A) cognitively unimpaired (CU) and B) cognitively impaired (CI) elderly individuals. Optimized ROC curves for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), *APOE*, clinical scores, plasma biomarkers ( $A\beta_{42}/A\beta_{40}$ , p-tau181, and NfL), and structural MRI-score when predicting  $A\beta$ -positivity using florbetapir PET as the ground truth in the ADNI study ( $n=333$  CUs and  $n=519$  CIs). To assess the added value of each class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI-score. Models including plasma  $A\beta_{42}/A\beta_{40}$  were tested and validated in a cohort of  $n=87$  CUs and  $n=86$  CIs due to limited available of plasma  $A\beta_{42}/A\beta_{40}$  data. Error bars indicate union of 95% CIs from cross-validation iterations.

Figure 3. Classifier performance metrics of  $A\beta$  positivity prediction in A) cognitively unimpaired (CU) individuals and B) individuals with mild cognitively impairment (CI). Area under the curve (AUC) estimates with  $\pm 2$  x standard variation error bars from cross-validation iterations are shown for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), *APOE*, clinical scores, plasma biomarkers ( $A\beta_{42}/A\beta_{40}$ , p-tau181, and NfL), and structural MRI-score when predicting  $A\beta$ -positivity using florbetapir PET as the

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3 ground truth in the ADNI study (n=333 CUs and n=519 CIs). To assess the added value of each  
4 class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were  
5 constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical  
6 features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with  
7 clinical features and MRI-score. Models including plasma  $A\beta_{42}/A\beta_{40}$  were tested and validated  
8 in a cohort of n=87 CUs and n=86 CIs due to limited available of plasma  $A\beta_{42}/A\beta_{40}$  data. Error  
9 bars indicate union of 95% CIs from cross-validation iterations.  
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## Supplementary Materials

### A $\beta$ PET imaging

The radiochemical synthesis of florbetapir for A $\beta$  PET imaging was overseen and regulated by Avid Radiopharmaceuticals and distributed to the qualifying ADNI sites. PET imaging was performed at each ADNI site according to standardized protocols, as described online (<http://adni.loni.usc.edu/methods/pet-analysis-method/pet-analysis/>). All PET scans underwent a rigorous quality control protocol and were processed to produce final images with standard orientation and voxel size of 2 mm<sup>3</sup> (Jagust *et al.*, 2015).

### Apolipoprotein E (*APOE*) genotyping

For ADNI-1 DNA samples, *APOE* genotyping was carried out by polymerase chain reaction (PCR) amplification, HhaI restriction enzyme digestion, and subsequent standard gel resolution and visualization processes (Hixson and Vernier, 1990; Reymer *et al.*, 1995). For ADNI-GO and ADNI-2 DNA samples, genotyping was performed by Prevention Genetics (Marshfield, WI, USA) and LGC Genomics (Beverly, MA, USA), employing array processing using allele-specific PCR with universal molecular beacons and competitive allele-specific PCR, enabling bi-allelic scoring of single nucleotide polymorphisms (SNPs), respectively (Myakishev *et al.*, 2001; Hawkins *et al.*, 2002).

### Plasma sample collection

The plasma samples were collected at the participating ADNI centers. After overnight fasting, plasma was collected in the morning by venipuncture into Vacutainer tubes (Becton Dickenson, Franklin Lakes, NJ) containing potassium K3 ethylene tetraacetate as an anticoagulant. After centrifugation, samples were placed in transfer tubes (13 mL polypropylene, Sarstedt Inc., Newton, NC, catalog number 60.541), frozen, and shipped on dry ice to the UPenn Biomarker Core Laboratory, where they were stored temporarily at  $-80^{\circ}\text{C}$ . The average time from blood collection to freezing of plasma for shipment was  $67 \pm 41$  minutes (95% confidence interval [CI]: 21–180 minutes). Within several weeks of receipt, the samples were thawed, aliquoted by

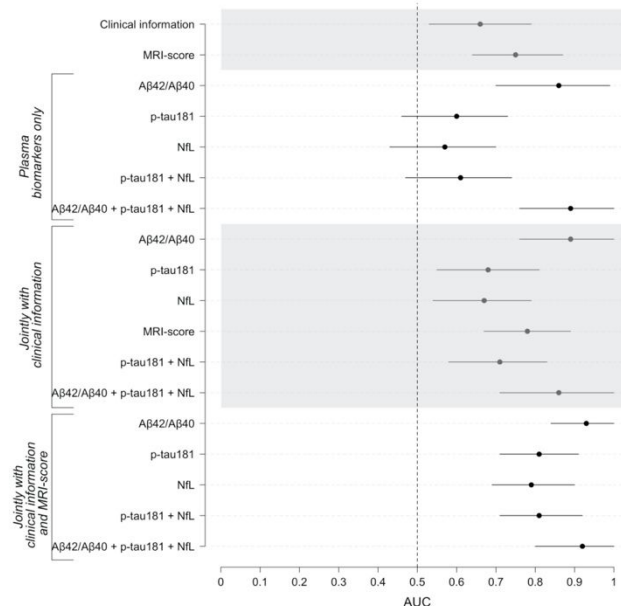
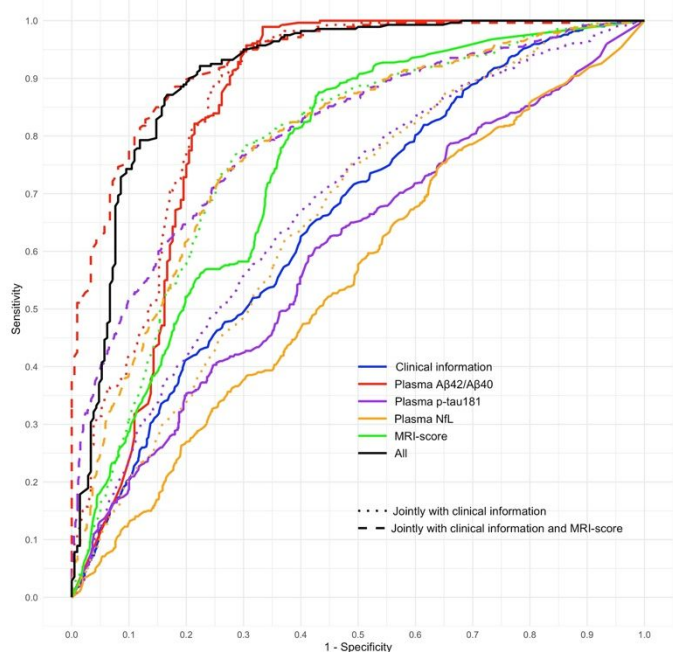
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3 500  $\mu$ L into aliquot tubes (1.5 mL polypropylene, Thermo Fisher Scientific, Waltham, MA,  
4 catalog number 05-408-129), and stored at  $-80^{\circ}\text{C}$  pending biochemical analyses.  
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### 9 **ADNI Plasma $\text{A}\beta_{42}$ and $\text{A}\beta_{40}$ processing**

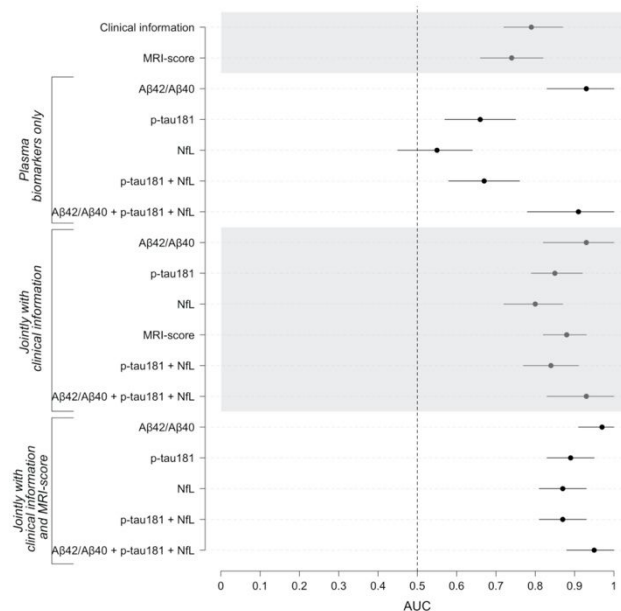
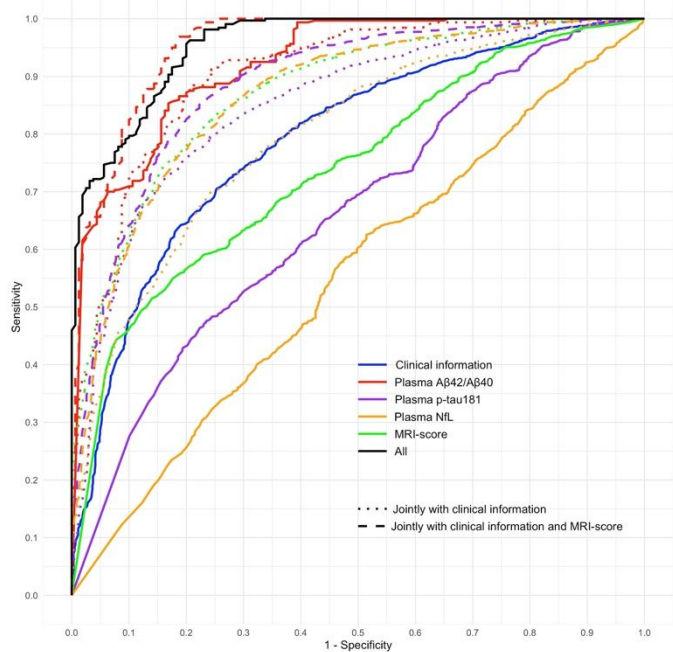
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12 Due to issues like ‘clogging’ on LC/MS and contamination noise signal on MS detector, three  
13 ADNI specific processing steps were implemented and validated, as follows:  
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- 15 1. Ion trap filtering MS method, which allows quant lower amount of  $\text{A}\beta$  isoforms.
- 16 2. Decrease the plasma volume from 1.8mL to 0.45mL – reducing matrix effect, while  
17 maintaining signal strong enough for required accuracy.
- 18 3. Centrifugation prior to immunoprecipitation and using automated immunoprecipitation  
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Cognitively unimpaired (CU) cohort



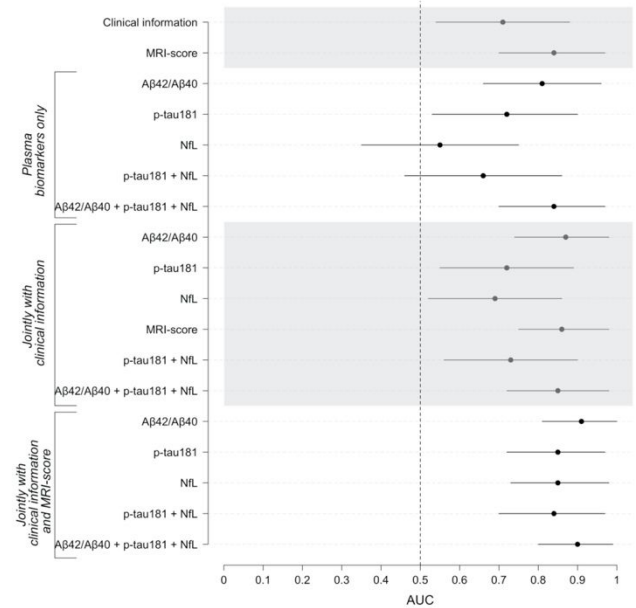
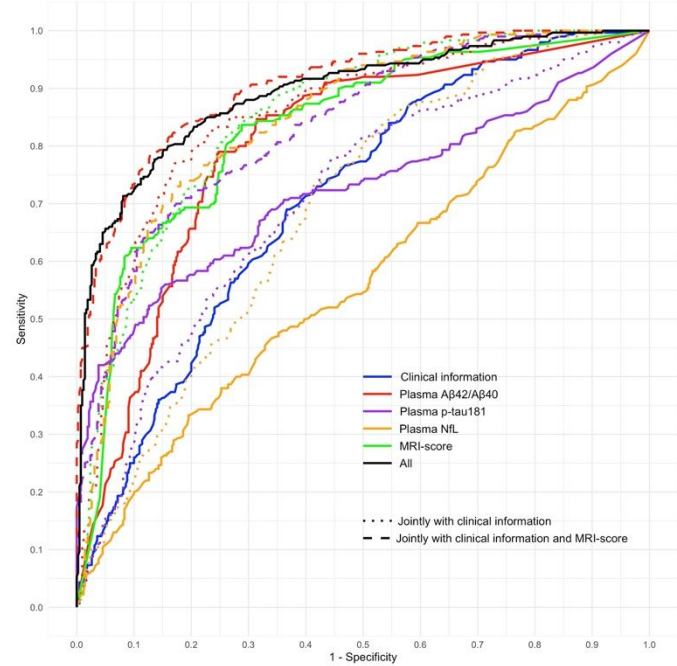
Mild cognitive impairment (CI) cohort



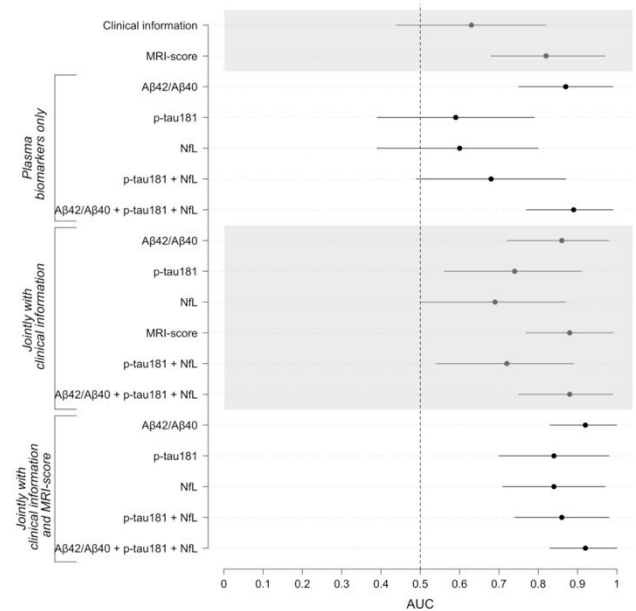
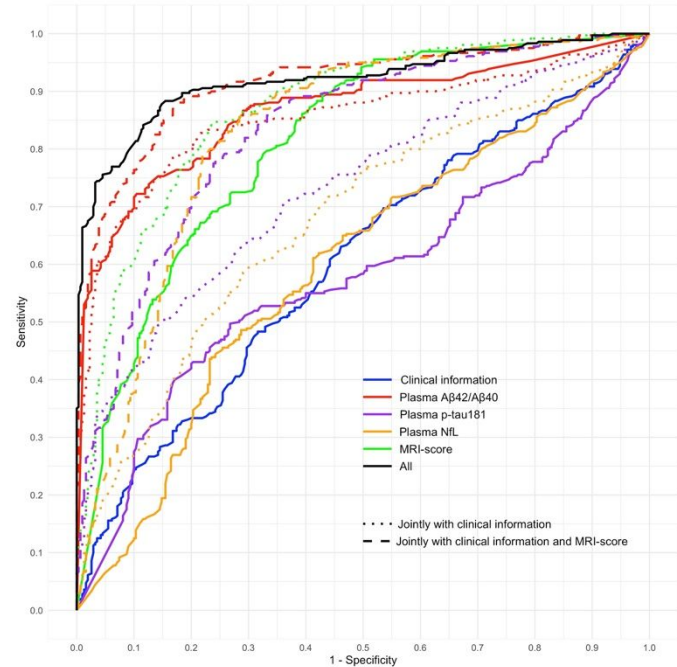
**Supp Figure 1. Performance with CSF Aβ-positivity as the ground truth:** Receiver operating characteristic (ROC) analysis of Aβ positivity prediction in an ADNI cohort of a) cognitively unimpaired (CU) individuals and b) individuals with mild cognitive impairment (CI). Optimized ROC curves and corresponding areas under the curve (AUCs) for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), *APOE*, clinical scores, plasma biomarkers (Aβ<sub>42</sub>/Aβ<sub>40</sub>, p-tau181, and NfL), and structural MRI-score when predicting Aβ-positivity using PET Aβ as the ground truth in the ADNI study. Error bars indicate union of 95% CIs from cross-validation iterations.



## Cognitively unimpaired (CU) cohort



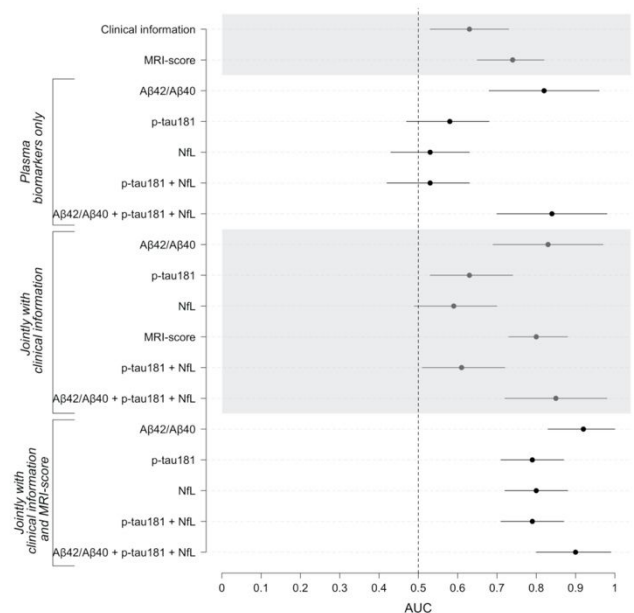
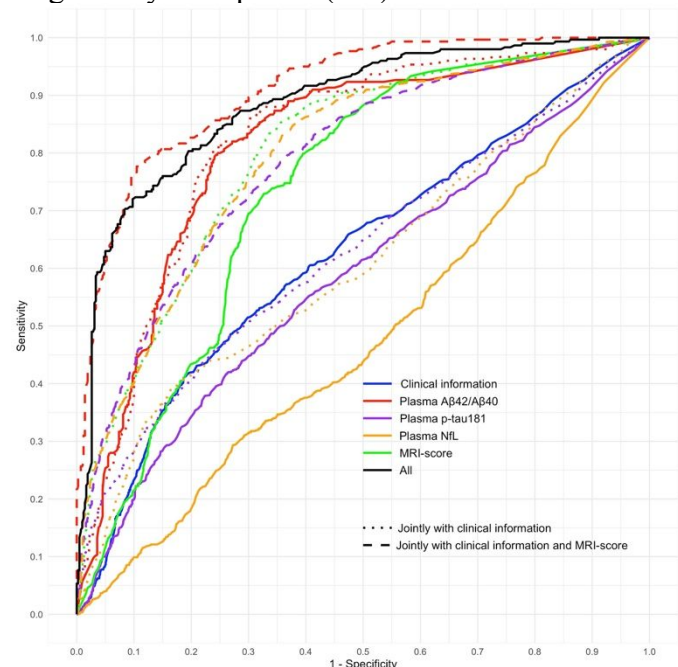
## Mild cognitive impairment (CI) cohort



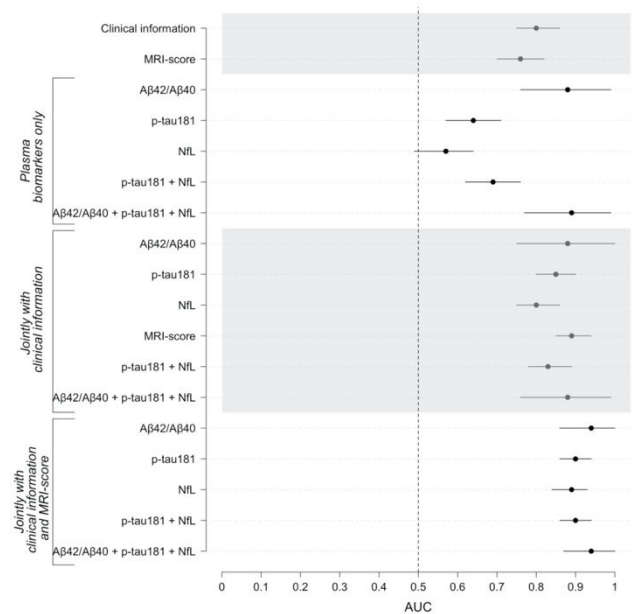
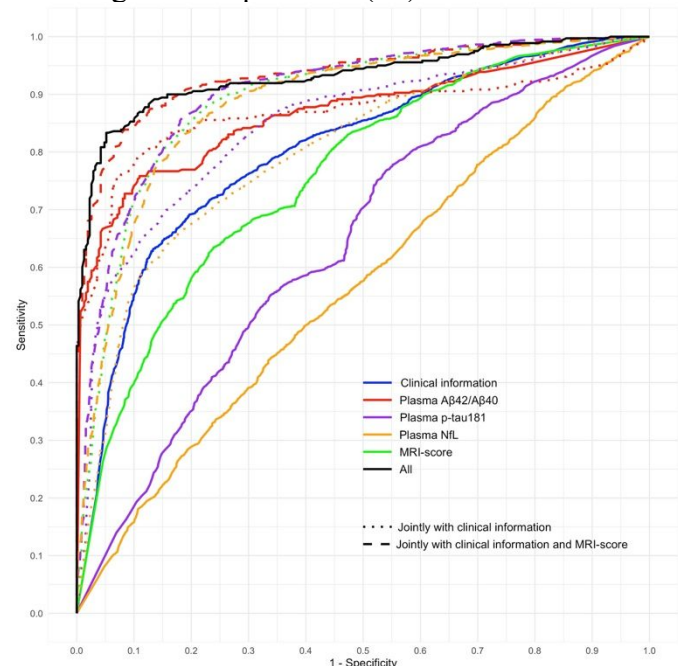
**Supp Figure 2. Performance with plasma  $A\beta_{42}/A\beta_{40}$  sub-cohort:** Receiver operating characteristic (ROC) analysis of  $A\beta$  positivity prediction in an ADNI cohort of a) cognitively unimpaired (CU) individuals and b) individuals with mild cognitive impairment (CI). Optimized ROC curves and corresponding areas under the curve (AUCs) for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), APOE, clinical scores, plasma biomarkers ( $A\beta_{42}/A\beta_{40}$ , p-tau181, and NfL), and structural MRI-score when predicting  $A\beta$ -positivity using florbetapir PET as the ground truth in the ADNI study. Models were limited to sub-cohort of cases with plasma  $A\beta_{42}/A\beta_{40}$  data, including  $n=87$  CUs and  $n=86$  CIs. Error bars indicate union of 95% CIs from cross-validation iterations.



Cognitively unimpaired (CU) cohort

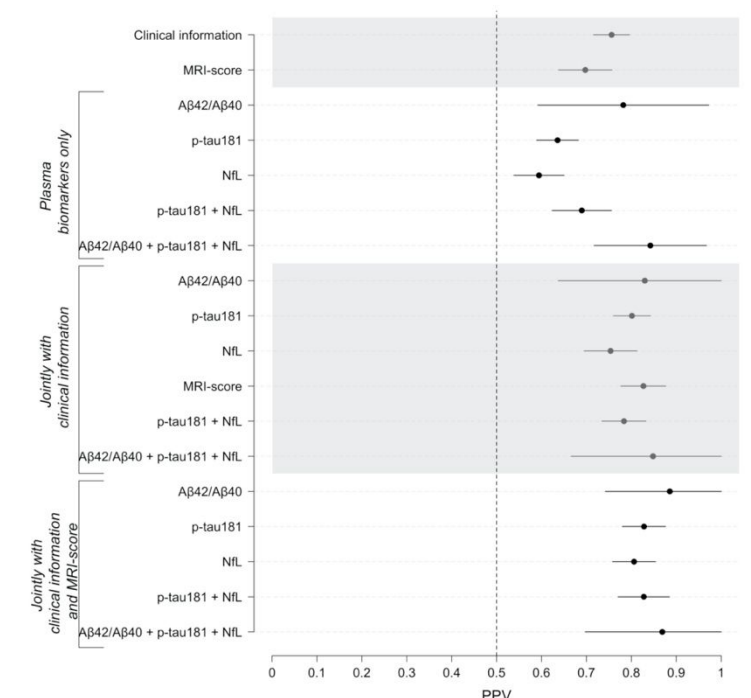
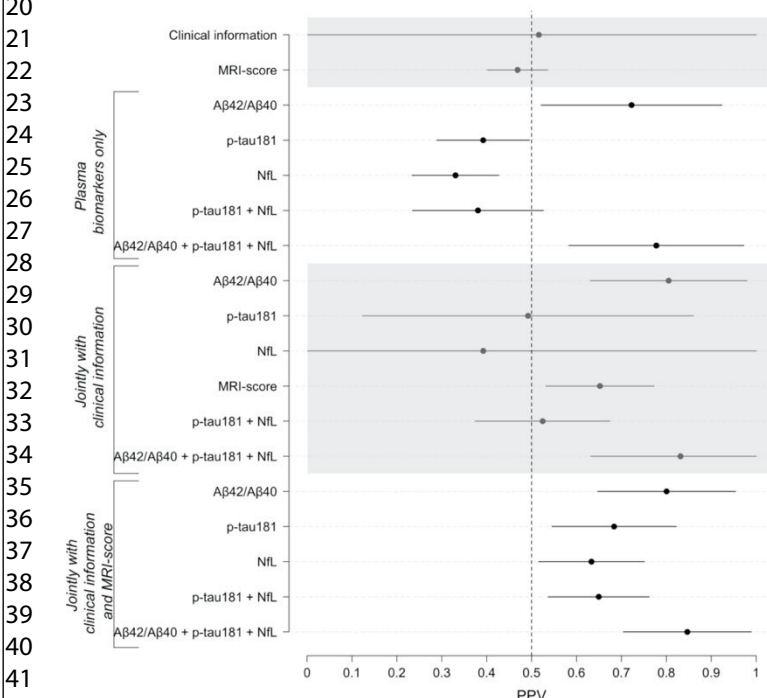
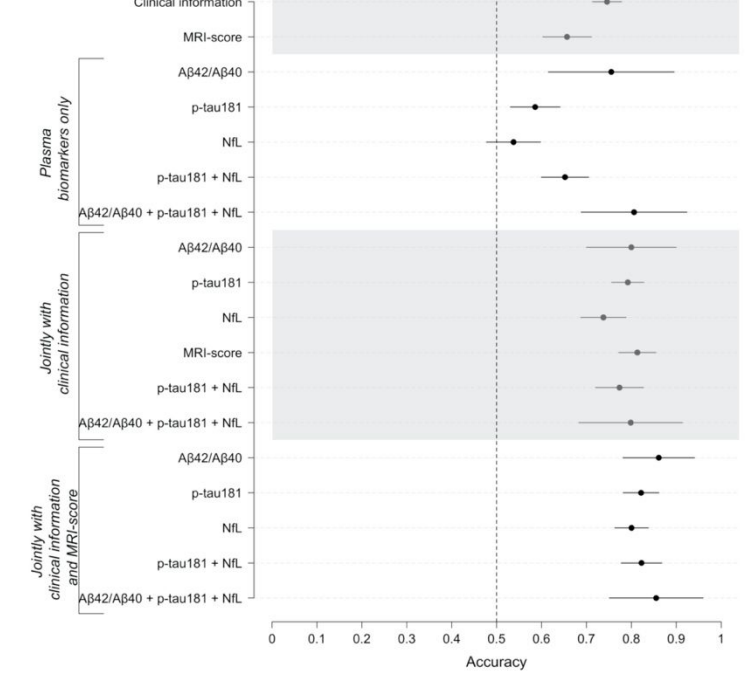
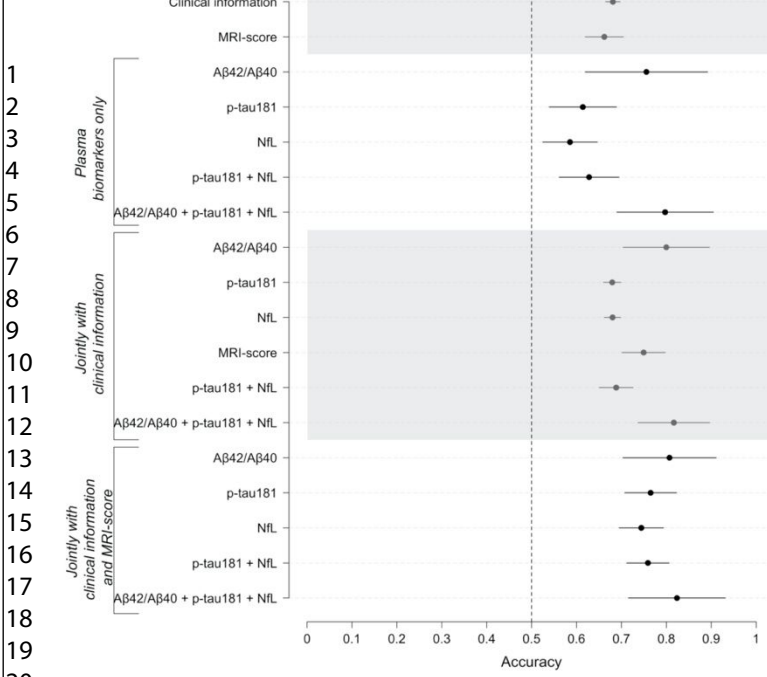


Mild cognitive impairment (CI) cohort

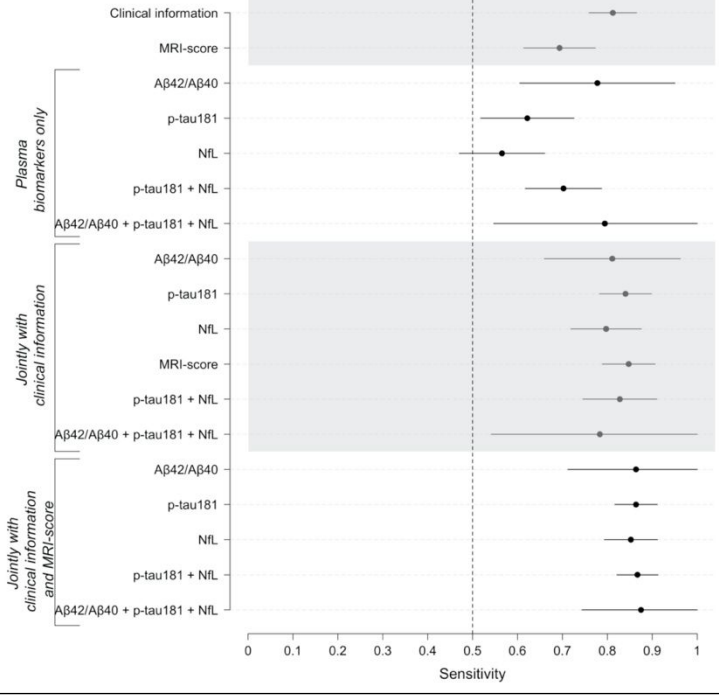
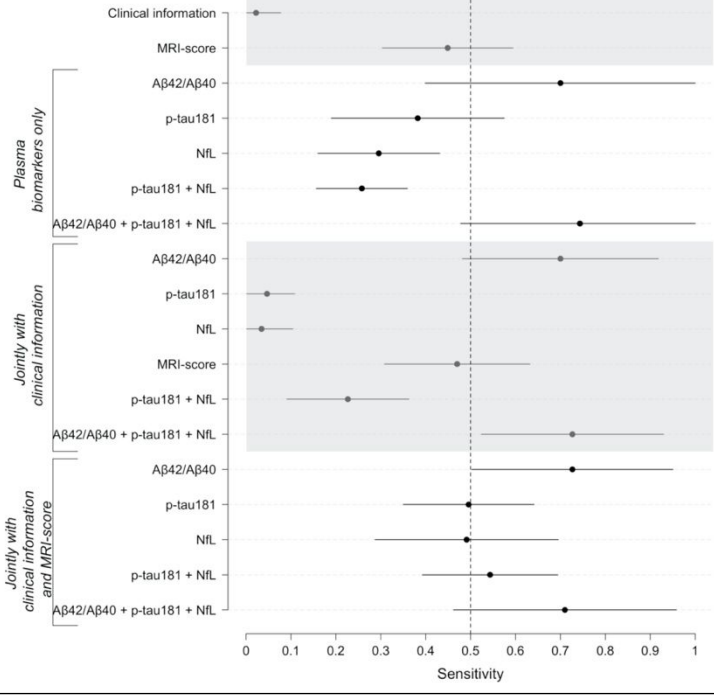
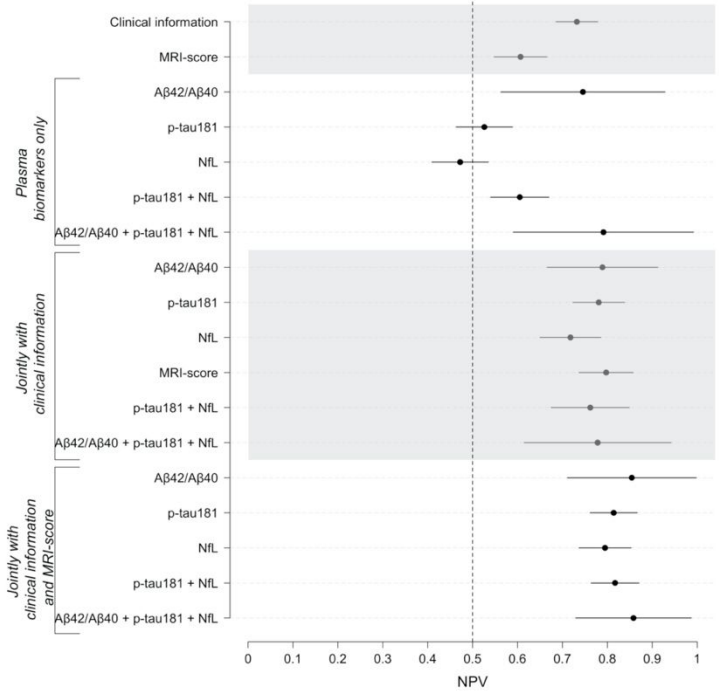
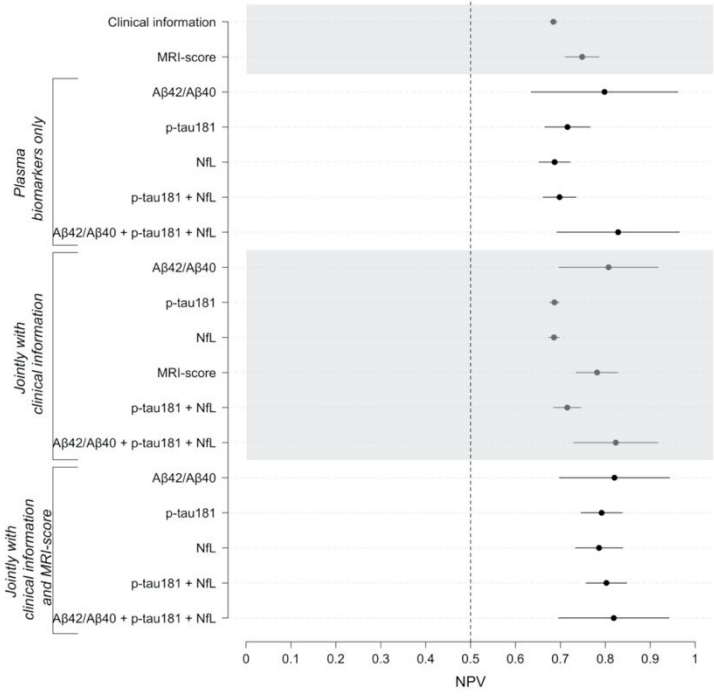


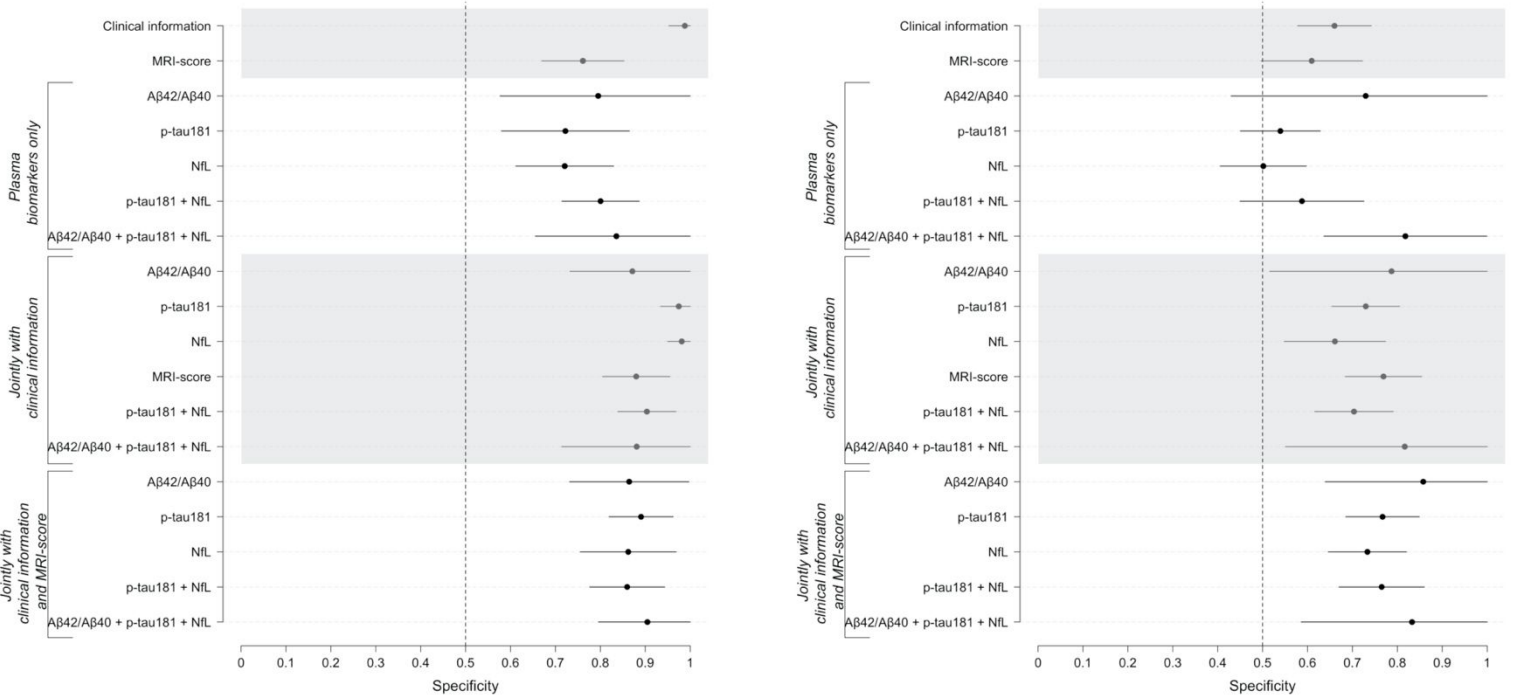
**Supp Figure 3. Performance with clinical information limited to age and APOE genotype:** Receiver operating characteristic (ROC) analysis of Aβ positivity prediction in an ADNI cohort of a) cognitively unimpaired (CU) individuals and b) individuals with mild cognitively impairment (CI). Optimized ROC curves and corresponding areas under the curve (AUCs) for classifiers constructed separately and jointly with clinical information (age and APOE only), plasma biomarkers (Aβ<sub>42</sub>/Aβ<sub>40</sub>, p-tau181, and NfL), and structural MRI-score when predicting Aβ-positivity using PET Aβ as the ground truth in the ADNI study. Error bars indicate union of 95% CIs from cross-validation iterations.

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**Supp Figure 4. Classifier performance metrics of Aβ positivity prediction in A) cognitively unimpaired (CU) individuals and B) individuals with mild cognitive impairment (CI). Classification accuracy, positive predictive value (PPV), negative predictive value (NPV), sensitivity, and specificity estimates with ± 2 x standard deviation error bars from cross-validation iterations are shown.**

## References

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	CU A $\beta$ -	CU A $\beta$ +	<i>p</i>	CI A $\beta$ -	CI A $\beta$ +	<i>p</i>
<i>Main cohort</i>						
N	224	109		230	289	
Age (years)	72.8 $\pm$ 6.2	74.6 $\pm$ 5.3	0.01	70.3 $\pm$ 7.9	73.3 $\pm$ 6.8	<10 <sup>-5</sup>
Sex (Female %)	52%	36%	0.005	56%	56%	
Education (years)	16.8 $\pm$ 2.5	15.9 $\pm$ 2.8	0.003	16.3 $\pm$ 2.5	15.9 $\pm$ 2.9	0.024
APOE $\epsilon$ 4 (carrier %)	21 %	43%	<10 <sup>-4</sup>	23%	66%	<10 <sup>-15</sup>
MMSE	29.1 $\pm$ 1.3	28.9 $\pm$ 1.1		28.4 $\pm$ 1.6	27.6 $\pm$ 1.8	<10 <sup>-6</sup>
CDR-SB	0.06 $\pm$ 0.2	0.1 $\pm$ 0.3	0.03	1.3 $\pm$ 0.8	1.6 $\pm$ 0.9	<10 <sup>-4</sup>
ADAS-Cog	5.5 $\pm$ 3.1	6.3 $\pm$ 3.0	0.02	7.8 $\pm$ 3.8	10.4 $\pm$ 4.6	<10 <sup>-10</sup>
Plasma NfL (pg/ml)	35.4 $\pm$ 15.8	39.4 $\pm$ 15.8	0.03	35.0 $\pm$ 18.7	43.3 $\pm$ 19.8	<10 <sup>-5</sup>
Plasma p-tau181 (pg/ml)	14.7 $\pm$ 10.6	16.9 $\pm$ 7.8		13.6 $\pm$ 8.6	21.6 $\pm$ 10.7	<10 <sup>-14</sup>
<i>Plasma A<math>\beta</math><sub>42</sub>/A<math>\beta</math><sub>40</sub> subcohort</i>						
N	50	37		40	46	
Age (years)	71.9 $\pm$ 6.1	75.3 $\pm$ 5.2	0.009	70.0 $\pm$ 7.9	73.1 $\pm$ 6.9	
Sex (Female %)	50%	33%		52%	51%	
Education (years)	16.8 $\pm$ 2.6	16.1 $\pm$ 2.4		16.4 $\pm$ 2.5	16.0 $\pm$ 3.0	
APOE $\epsilon$ 4 (carrier %)	14%	51%	0.001	22%	63%	0.002
MMSE	29.2 $\pm$ 1.0	28.9 $\pm$ 1.0		28.5 $\pm$ 1.3	27.6 $\pm$ 2.0	0.04
CDR-SB	0.04 $\pm$ 0.1	0.11 $\pm$ 0.2		0.8 $\pm$ 0.2	0.7 $\pm$ 0.2	
ADAS-Cog	5.5 $\pm$ 2.7	6.5 $\pm$ 3.1		7.0 $\pm$ 3.0	8.4 $\pm$ 3.4	
Plasma NfL (pg/ml)	32.1 $\pm$ 15.8	36.1 $\pm$ 12.3		30.8 $\pm$ 11.3	37.7 $\pm$ 14.7	0.04
Plasma p-tau181 (pg/ml)	13.5 $\pm$ 10.1	18.8 $\pm$ 7.7	0.01	14.5 $\pm$ 10.0	18.7 $\pm$ 7.6	
Plasma A $\beta$ <sub>42</sub> /A $\beta$ <sub>40</sub>	0.12 $\pm$ 0.01	0.11 $\pm$ 0.01	<10 <sup>-6</sup>	0.13 $\pm$ 0.01	0.11 $\pm$ 0.009	<10 <sup>-10</sup>

34 CU: Cognitively unimpaired elderly; CI: Elderly individuals with mild cognitive impairment;  
 35 APOE: Apolipoprotein E; MMSE: Mini-Mental State Examination; CDR-SB: Clinical Dementia  
 36 Rating – Sum of Boxes; ADAS-Cog: Alzheimer's Disease Assessment Scale – Cognitive  
 37 subscale 13-item; NfL: neurofilament light  
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3 Table 2. Performance of classifier models in classifying A $\beta$ + cognitively unimpaired (CU) individuals. To assess the added value of each class of variables  
 4 (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with  
 5 clinical features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI-score.

	(A) Plasma Biomarkers						(B) Clinical information with and without plasma biomarkers						(C) MRI-score with and without clinical information and plasma biomarkers					
	AUC <sup>†</sup>	Acc	PPV	NPV	Sens	Spec	AUC <sup>†</sup>	Acc	PPV	NPV	Sens	Spec	AUC <sup>†</sup>	Acc	PPV	NPV	Sens	Spec
9 MRI score													0.74	0.67	0.48	0.76	0.46	0.77
													[0.66,	±	±	±	±	±
													0.82]	0.04	0.06	0.03	0.11	0.04
11 Clinical							0.69	0.68	0.45	0.68	0.03	0.98	0.80	0.75	0.65	0.78	0.48	0.88
12 information*							[0.60,	±	±	±	±	±	[0.72,	±	±	±	±	±
							0.78]	0.01	0.28	0.01	0.03	0.01	0.87]	0.02	0.06	0.02	0.09	0.05
14 A $\beta$ <sub>42</sub> /A $\beta$ <sub>40</sub>	0.80	0.72	0.69	0.76	0.64	0.77	0.86	0.79	0.77	0.81	0.71	0.84	0.90	0.83	0.84	0.83	0.74	0.89
	[0.65,	±	±	±	±	±	[0.73,	±	±	±	±	±	[0.80,	±	±	±	±	±
	0.94]	0.07	0.12	0.08	0.18	0.13	0.98]	0.05	0.08	0.06	0.11	0.07	1.00]	0.04	0.08	0.05	0.10	0.06
16 P-tau181	0.55 <sup>‡</sup>	0.62	0.39	0.71	0.37	0.73	0.69	0.69	0.58	0.69	0.07	0.98	0.80	0.76	0.69	0.78	0.46	0.90
	[0.45,	±	±	±	±	±	[0.60,	±	±	±	±	±	[0.73,	±	±	±	±	±
	0.66]	0.02	0.04	0.02	0.07	0.05	0.78]	0.01	0.29	0.01	0.06	0.03	0.88]	0.03	0.07	0.02	0.06	0.04
19 NfL	0.54 <sup>‡</sup>	0.57	0.31	0.68	0.31	0.69	0.68	0.68	0.51	0.68	0.03	0.98	0.79	0.74	0.64	0.78	0.45	0.88
	[0.44,	±	±	±	±	±	[0.59,	±	±	±	±	±	[0.71,	±	±	±	±	±
	0.64]	0.03	0.05	0.02	0.08	0.04	0.77]	0.01	0.33	0.01	0.02	0.02	0.87]	0.03	0.06	0.02	0.06	0.04
22 P-tau181 +	0.53 <sup>‡</sup>	0.60	0.34	0.69	0.26	0.76	0.65	0.69	0.53	0.72	0.25	0.90	0.80	0.76	0.66	0.80	0.54	0.87
23 NfL	[0.42,	±	±	±	±	±	[0.56,	±	±	±	±	±	[0.72,	±	±	±	±	±
	0.63]	0.04	0.07	0.02	0.08	0.05	0.75]	0.03	0.10	0.02	0.08	0.04	0.88]	0.03	0.08	0.02	0.08	0.05
24 A $\beta$ <sub>42</sub> /A $\beta$ <sub>40</sub> +	0.83	0.77	0.77	0.80	0.70	0.83	0.85	0.81	0.82	0.83	0.73	0.87	0.91	0.82	0.90	0.79	0.63	0.95
25 p-tau181 +	[0.68,	±	±	±	±	±	[0.72,	±	±	±	±	±	[0.81,	±	±	±	±	±
26 NfL	0.97]	0.06	0.13	0.06	0.12	0.14	0.98]	0.04	0.08	0.06	0.11	0.08	0.99]	0.06	0.08	0.07	0.14	0.04

27\* Demographics: Age, sex, years of education, and APOE  $\epsilon$ 4 status; Global cognitive assessments: MMSE, ADAS-Cog, and CDR-SB

28<sup>†</sup> 95% confidence intervals

29<sup>‡</sup> The confidence interval includes the axis y=x, suggesting that the classifier was not better than chance.

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Table 3. Performance of classifier models in differentiating Aβ+ individuals with mild cognitive impairment (CI). To assess the added value of each class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI-score.

	(A) Plasma biomarkers						(B) Clinical information with and without plasma biomarkers						(C) MRI-score with and without clinical information and plasma biomarkers					
	AUC †	Acc	PPV	NPV	Sens	Spec	AUC †	Acc	PPV	NPV	Sens	Spec	AUC †	Acc	PPV	NPV	Sens	Spec
MRI score													0.76	0.67	0.70	0.63	0.72	0.61
													[0.70, ± 0.02]	± 0.02	± 0.02	± 0.03	± 0.03	± 0.04
Demographics							0.81	0.74	0.76	0.73	0.81	0.66	0.88	0.81	0.82	0.80	0.85	0.76
+ Clinical *							[0.75, ± 0.02]	± 0.02	± 0.02	± 0.03	± 0.03	± 0.05	[0.83, ± 0.02]	± 0.02	± 0.03	± 0.03	± 0.03	± 0.04
Aβ42/Aβ40	0.87	0.77	0.79	0.76	0.79	0.75	0.85	0.79	0.81	0.77	0.80	0.77	0.94	0.86	0.86	0.88	0.90	0.82
	[0.75, ± 0.06]	± 0.06	± 0.07	± 0.08	± 0.08	± 0.10	[0.71, ± 0.05]	± 0.05	± 0.10	± 0.06	± 0.07	± 0.14	[0.87, ± 1.00]	± 0.05	± 0.07	± 0.08	± 0.07	± 0.1
p-tau181	0.64	0.58	0.63	0.52	0.61	0.55	0.85	0.79	0.80	0.78	0.83	0.73	0.90	0.82	0.83	0.82	0.86	0.78
	[0.56, ± 0.03]	± 0.03	± 0.02	± 0.03	± 0.05	± 0.05	[0.80, ± 0.02]	± 0.02	± 0.02	± 0.04	± 0.04	± 0.03	[0.86, ± 0.94]	± 0.02	± 0.01	± 0.04	± 0.03	± 0.02
NfL	0.56‡	0.54	0.60	0.48	0.57	0.51	0.81	0.73	0.75	0.71	0.79	0.66	0.87	0.81	0.82	0.79	0.85	0.75
	[0.49, ± 0.03]	± 0.03	± 0.02	± 0.03	± 0.03	± 0.04	[0.75, ± 0.02]	± 0.02	± 0.03	± 0.03	± 0.04	± 0.05	[0.83, ± 0.92]	± 0.02	± 0.03	± 0.02	± 0.03	± 0.06
p-tau181 + NfL	0.70	0.66	0.69	0.62	0.72	0.58	0.84	0.77	0.78	0.76	0.83	0.70	0.89	0.82	0.83	0.81	0.86	0.77
	[0.63, ± 0.02]	± 0.02	± 0.02	± 0.02	± 0.03	± 0.05	[0.79, ± 0.03]	± 0.03	± 0.03	± 0.04	± 0.04	± 0.06	[0.85, ± 0.93]	± 0.02	± 0.03	± 0.03	± 0.03	± 0.05
Aβ42/Aβ40 + p-tau181 + NfL	0.88	0.80	0.81	0.81	0.84	0.76	0.89	0.82	0.85	0.81	0.83	0.82	0.92	0.86	0.88	0.86	0.87	0.86
	[0.76, ± 0.05]	± 0.05	± 0.07	± 0.08	± 0.09	± 0.11	[0.78, ± 1.00]	± 0.06	± 0.10	± 0.07	± 0.07	± 0.13	[0.82, ± 1.00]	± 0.05	± 0.07	± 0.06	± 0.05	± 0.09

\* Demographics: Age, sex, years of education, and APOE ε4 status; Clinical assessments: MMSE, ADAS-Cog, and CDR-SB

† 95% confidence intervals

‡ The confidence interval includes the axis y=x, suggesting that the classifier was not better than chance.

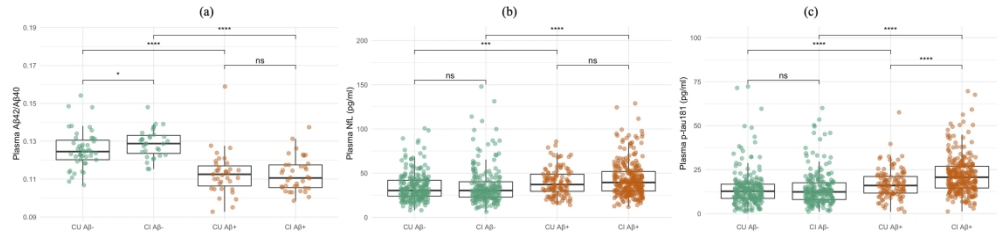


Figure 1. Plasma a) A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub>, b) NfL concentrations, and c) p-tau181 concentrations categorized by clinical diagnosis and CSF A $\beta$ -positivity. Plasma A $\beta$ <sub>42</sub>/A $\beta$ <sub>40</sub> data was available for 173 individuals (A $\beta$ <sup>-</sup> CU, n=50; A $\beta$ <sup>+</sup> CU, n=37; A $\beta$ <sup>-</sup> CI, n=40; A $\beta$ <sup>+</sup> CI, n=46). Plasma p-tau181 and NfL data included 852 individuals (A $\beta$ <sup>-</sup> CU, n=224; A $\beta$ <sup>+</sup> CU, n=109; A $\beta$ <sup>-</sup> CI, n=230; A $\beta$ <sup>+</sup> CI, n=289). Unpaired two-samples t-test uncorrected significance levels at \*\*\*\*: p<0.00001; \*\*\*: p<0.0001; \*\*: p<0.001; ns: p  $\geq$  0.5. CU: Cognitively unimpaired elderly; CI: Elderly individuals with mild cognitive impairment.

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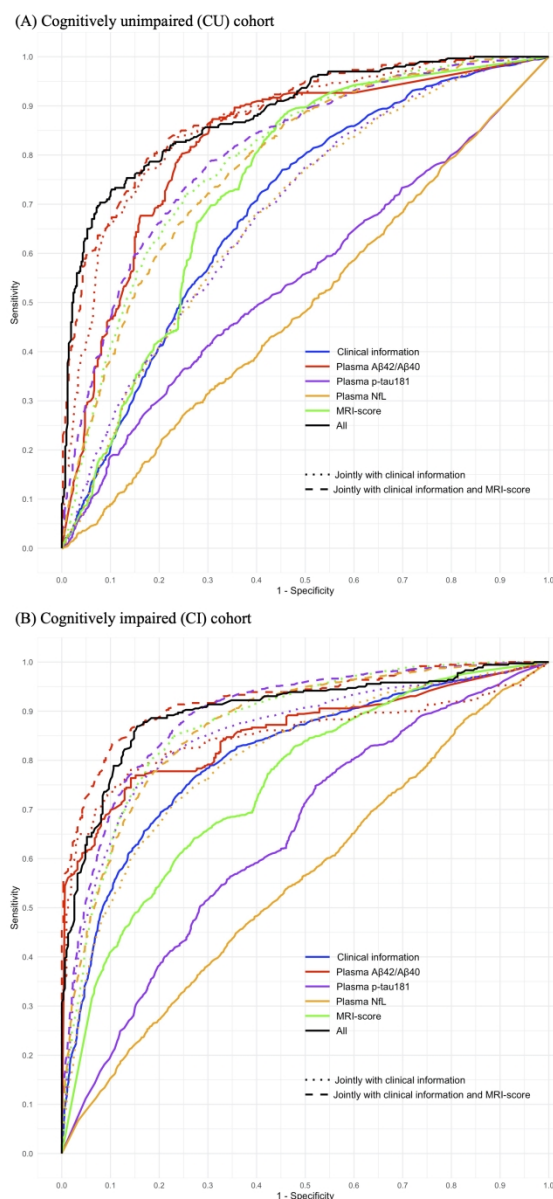


Figure 2. Receiver operating characteristic (ROC) analysis of A $\beta$  positivity prediction in an ADNI cohort of A) cognitively unimpaired (CU) and B) cognitively impaired (CI) elderly individuals. Optimized ROC curves for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), APOE, clinical scores, plasma biomarkers (A $\beta$ 42/A $\beta$ 40, p-tau181, and NfL), and structural MRI-score when predicting A $\beta$ -positivity using florbetapir PET as the ground truth in the ADNI study (n=333 CUs and n=519 CIs). To assess the added value of each class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI-score. Models including plasma A $\beta$ 42/A $\beta$ 40 were tested and validated in a cohort of n=87 CUs and n=86 CIs due to limited available of plasma A $\beta$ 42/A $\beta$ 40 data. Error bars indicate union of 95% CIs from cross-validation iterations.

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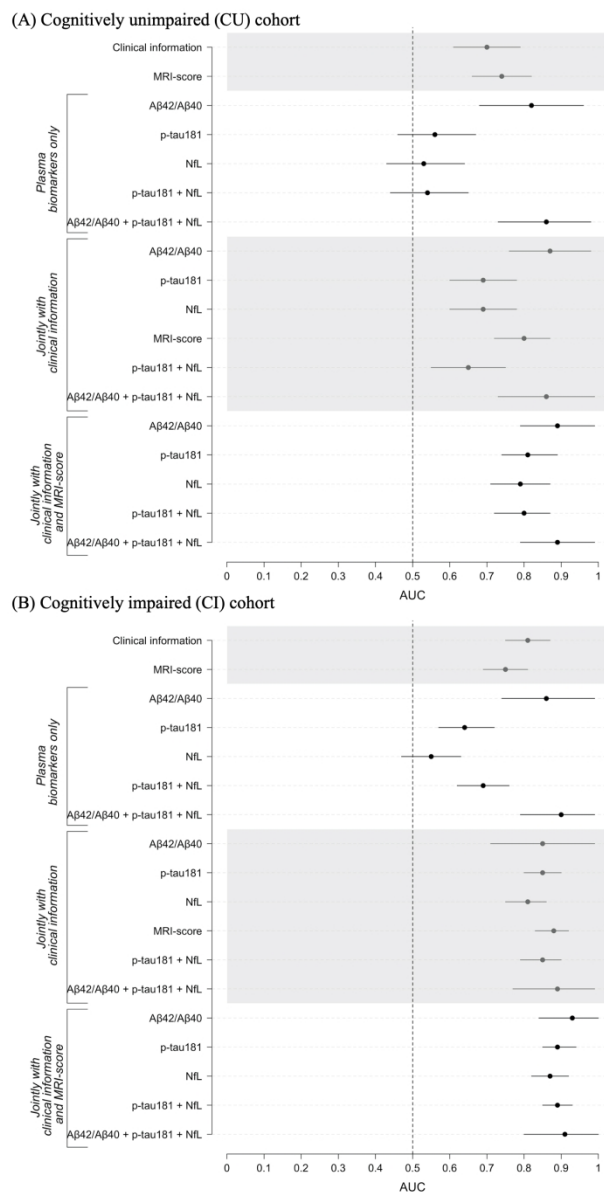


Figure 3. Classifier performance metrics of Aβ positivity prediction in A) cognitively unimpaired (CU) individuals and B) individuals with mild cognitively impairment (CI). Area under the curve (AUC) estimates with ± 2 x standard variation error bars from cross-validation iterations are shown for classifiers constructed separately and jointly with demographic information (age, sex, and years of education), APOE, clinical scores, plasma biomarkers (Aβ42/Aβ40, p-tau181, and NfL), and structural MRI-score when predicting Aβ-positivity using florbetapir PET as the ground truth in the ADNI study (n=333 CUs and n=519 CIs). To assess the added value of each class of variables (i.e., clinical, plasma, and MRI classes), additional RF classifiers were constructed from 1) each plasma marker alone, 2) each plasma marker jointly with clinical features, 3) MRI-score jointly with clinical features, and 4) each plasma marker jointly with clinical features and MRI-score. Models including plasma Aβ42/Aβ40 were tested and validated in a cohort of n=87 CUs and n=86 CIs due to limited available of plasma Aβ42/Aβ40 data. Error bars indicate union of 95% CIs from cross-validation iterations.

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